



US008734341B2

(12) **United States Patent**
Howell et al.

(10) **Patent No.:** **US 8,734,341 B2**
(45) **Date of Patent:** **May 27, 2014**

(54) **METHOD AND APPARATUS TO SENSE
HYDRATION LEVEL OF A PERSON**

600/362, 366, 367, 370-371, 393, 549, 529,
600/551, 573, 582, 581; 73/32 R, 434, 453,
73/73, 861, 861.05, 861.12, 204.25, 272 R,
73/861.14; 436/43, 44, 54, 182, 805, 807,
436/810, 811, 812, 815, 900, 901, 906;
324/425, 426, 439, 446

(75) Inventors: **Thomas A. Howell**, Palo Alto, CA (US);
Angeline Hadiwidjaja, Los Altos, CA
(US); **Peter P. Tong**, Mountain View, CA
(US); **C. Douglass Thomas**, Campbell,
CA (US)

See application file for complete search history.

(73) Assignee: **IpVenture, Inc.**, Los Altos, CA (US)

(56) **References Cited**

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 1697 days.

U.S. PATENT DOCUMENTS

3,420,205 A * 1/1969 Morison 116/200
4,126,132 A 11/1978 Portner et al.

(Continued)

(21) Appl. No.: **11/592,431**

FOREIGN PATENT DOCUMENTS

(22) Filed: **Nov. 2, 2006**

EP 0 274 363 B1 7/1988
EP 1 184 663 A3 3/2002
WO WO 2005084531 A1 * 9/2005

(65) **Prior Publication Data**

US 2007/0048224 A1 Mar. 1, 2007

OTHER PUBLICATIONS

Related U.S. Application Data

Murray, R. in "Dehydration, Hyperthermia, and Athletes: Science
and Practice", Journal of Athletic Training, vol. 31, No. 3, Sep. 1996,
p. 248-249.*

(63) Continuation-in-part of application No. 11/451,781,
filed on Jun. 12, 2006, now abandoned, which is a

(Continued)

(Continued)

Primary Examiner — Gary Jackson
Assistant Examiner — Marie Archer

(51) **Int. Cl.**

A61B 5/00 (2006.01)
A61B 10/00 (2006.01)
G01N 21/78 (2006.01)
G01N 37/00 (2006.01)

(57) **ABSTRACT**

A hydration sensor or sensing element configured to measure
the hydration level of a user is disclosed. The sensing element
can include a water-permeable material positioned in
between two water-impermeable material. The sensing ele-
ment can be coupled to a bottle of fluid, or a carrier with a
timer. The sensing element can be incorporated into a hand-
held device. The sensing element can be a disposable ele-
ment, an element applicable for more than one-time use, or a
re-usable element. The sensing element or sensor can be
calibrated for a specific user or a group of users. One or more
additional sensors that do not measure hydration level of the
user can be coupled to a hydration sensing element to deter-
mine the amount of fluid consumption for the user in different
conditions.

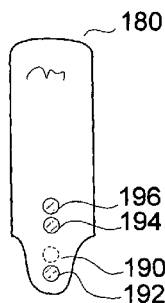
(52) **U.S. Cl.**

CPC **A61B 5/4875** (2013.01); **A61B 10/0045**
(2013.01); **A61B 10/0051** (2013.01); **A61B**
5/6802 (2013.01); **G01N 21/78** (2013.01);
G01N 37/005 (2013.01); **A61B 2562/0295**
(2013.01); **B01L 2300/0825** (2013.01)
USPC **600/300**; 429/9.1; 73/53.01; 600/573;
600/309; 436/162; 436/164; 436/169; 436/170;
436/172; 436/180; 422/401

(58) **Field of Classification Search**

USPC 600/300-301, 306-308, 325, 346, 349,

16 Claims, 18 Drawing Sheets



Related U.S. Application Data

- (63) continuation-in-part of application No. 11/314,545, filed on Dec. 20, 2005, now abandoned.
- (60) Provisional application No. 60/636,969, filed on Dec. 20, 2004, provisional application No. 60/652,213, filed on Feb. 14, 2005, provisional application No. 60/670,957, filed on Apr. 13, 2005, provisional application No. 60/689,312, filed on Jun. 10, 2005, provisional application No. 60/732,925, filed on Nov. 2, 2005, provisional application No. 60/785,825, filed on Mar. 24, 2006.

References Cited

(56)

U.S. PATENT DOCUMENTS

4,513,608	A	4/1985	Cuming	
4,860,753	A	8/1989	Amerena	
4,883,063	A	11/1989	Bernard et al.	
5,014,798	A	5/1991	Glynn	
5,231,993	A	8/1993	Haber et al.	
5,353,802	A	10/1994	Ollmar	
5,426,415	A	6/1995	Prachar et al.	
5,495,961	A	3/1996	Maestre	
5,563,584	A	10/1996	Rader et al.	
5,580,794	A *	12/1996	Allen	436/169
5,755,672	A	5/1998	Arai et al.	
5,833,625	A	11/1998	Essen-Moller	
5,834,691	A *	11/1998	Aoki	174/529
5,938,593	A	8/1999	Ouellette	
6,107,537	A	8/2000	Elder et al.	
6,248,067	B1	6/2001	Causey, III et al.	
6,319,199	B1	11/2001	Sheehan et al.	
6,370,426	B1	4/2002	Campbell et al.	
6,466,821	B1	10/2002	Pianca et al.	
6,485,982	B1	11/2002	Charlton	
6,523,392	B2	2/2003	Porter et al.	
6,529,446	B1	3/2003	de la Huerga	
6,529,767	B1	3/2003	Woo et al.	
6,569,094	B2	5/2003	Suzuki et al.	
6,602,469	B1	8/2003	Maus et al.	
6,623,698	B2	9/2003	Kuo	
6,780,307	B2	8/2004	Kidwell	
6,823,717	B2	11/2004	Porter et al.	
6,854,317	B2	2/2005	Porter et al.	
6,998,273	B1 *	2/2006	Fleming et al.	436/514
7,170,823	B2	1/2007	Fabricius et al.	
7,273,454	B2 *	9/2007	Raymond et al.	600/301
7,323,141	B2	1/2008	Kirchhevel et al.	
7,332,642	B2 *	2/2008	Liu	604/361
2002/0001852	A1 *	1/2002	Mendel-Hartvig et al.	436/514
2002/0147617	A1	10/2002	Schoenbaum et al.	
2003/0002238	A1	1/2003	Toyoda	
2004/0121478	A1 *	6/2004	Brinz et al.	436/109
2004/0133081	A1	7/2004	Teller et al.	
2005/0033200	A1 *	2/2005	Soehren et al.	600/595
2005/0143675	A1	6/2005	Neel et al.	
2005/0169810	A1 *	8/2005	Hagen et al.	422/102
2005/0228692	A1	10/2005	Hodgdon	
2006/0121548	A1 *	6/2006	Robbins et al.	435/18
2006/0231109	A1	10/2006	Howell et al.	
2006/0241355	A1	10/2006	Howell et al.	
2006/0248946	A1	11/2006	Howell et al.	
2006/0278156	A1 *	12/2006	Miller	116/112
2007/0024465	A1	2/2007	Howell et al.	
2007/0213606	A1	9/2007	Sherman et al.	
2007/0225578	A1	9/2007	Howell et al.	
2007/0249059	A1	10/2007	Stewart	
2008/0025154	A1 *	1/2008	MacDonald et al.	368/89
2008/0146890	A1	6/2008	LeBoeuf et al.	

OTHER PUBLICATIONS

Prince, R. "A disposable, self-administered Electrolyte Test", submitted to the Department of Electrical Engineering and Computer

Science in partial fulfillment of the requirements for the degree of Master of Engineering in Electrical Engineering at the Massachusetts Institute of Technology, Feb. 2003, p. 13-17.*

Casa, D. J. et al in "National Athletic Trainers' Association Position Statement: Fluid Replacement for Athletes", Journal of Athletic Training, 2003, vol. 35, No. 2, p. 212-224.*

Helton, K.L. et al. "Interfacial instabilities affect microfluidic extraction of small molecules from non-Newtonian fluids", Lab Chip, 2007, 7, 1581-1588.*

Renner-Nantz J. in Current Protocols in Food Analytical Chemistry (2001) H1.3.1-H1.3.5, 2001 by John Wiley & Sons, Inc.*

Sikdar, S. et al in "Viscosity Measurements of Non-Newtonian Slurry Suspensions Using Rotating Viscometers", Ind. Eng. Chem. Process Des. Dev., vol. 18, No. 4, 1979, p. 722-726.*

Walsh, N. P. et al. "Saliva flow rate, total protein concentration and osmolality as potential markers of whole body hydration status during progressive acute dehydration in humans", Archives of Oral Biology (2004) 49, 149-154.*

Cheuvront, S. N. et al. "Hydration Assessment of Athletes", Sports Science Exchange 97, vol. 18, No. 2, 2005, p. 1-12.*

"Comparison of a New Test for the Measurement of Resting Whole Saliva with the Draining and the Swab Techniques", Pia López-Jornet et al., Department of Oral Medicine, University of Murcia, Murcia, Spain, electronic publication: Feb. 1997, 6 pages.

"Hydration status measurement by radio frequency absorptiometry in young athletes, a new method and preliminary results," Daniel S. Moran et al., *loP electronic journals, Psychosocial Measurement*, Feb. 2004, pp. 51-59.

"Sensing device that when implanted in the mouth can detect hydration levels in soldiers", News-Medical.net, Devices/Technology, May 18, 2004, 3 pages.

"Xerostomia Information for dentists, Helping patients with dry mouth", Bartels, Cathy L., <http://www.oralcancerfoundation.org/dental/xerostomia.htm>, downloaded Mar. 22, 2007, pp. 1-14.

"0136 A new method to measure viscosity in saliva", Becker, K., et al., http://iadr.confex.com/iadr/eur05/techprogram/abstract_67646.htm, downloaded Oct. 14, 2005, pp. 1.

BiODE, Technical White Paper #1, (undated) downloaded Dec. 6, 2006, pp. 1-2.

Brownlee, Christen, "Oral Exams, Saliva could provide an alternative for some diagnostic tests," *www.sciencenews.org*, vol. 168, Sep. 17, 2005, pp. 187-188.

Cambridge Viscometers: Accurate, Reliable and Proven Fluid Viscosity Measurement Technology, <http://www.cambridgeviscosity.com/default.aspx>, downloaded Dec. 6, 2006, p. 1.

Marketing Devices, http://www.courage-khazaka.de/products/marketing_products.htm, downloaded May 14, 2007, pp. 1-4.

Products for Dermatology, http://www.courage-khazaka.de/products/derma_products.htm, downloaded May 14, 2007, pp. 1-4.

Scientific Devices, http://www.courage-khazaka.de/products/scientific_rd_prod.htm, downloaded May 14, 2007, pp. 1-5.

"Easily check the skin's moisture content," pp. 32-33.

e-pill Pill Bottle Multi Alarm, <http://www.epill.com/bottle.html>, downloaded Dec. 5, 2006.

Étude, "The Way to skin counseling," Operation Manual, undated, front cover page and pp. 1-27.

GOJO Skin Care Lab, Fast, Effective Hand Cleaning, http://automotive.gojo.com/skin_care/, downloaded Nov. 29, 2006, pp. 1-2.

"L'Oréal and STMicroelectronics applying semiconductors to skin aging," Press Release, Geneva, Oct. 18, 2002, pp. 2.

LifePoint Inc.—Saliva Based Testing Systems for the next generation, LifePoint® IMPACT® Test System, undated, 2 pages.

Moritex USA Incorporated, Sensors & Meters, copyright 2004, http://www.moritexusa.com/products/product_category.php?plid=5&pcid=10, downloaded Apr. 19, 2006, pp. 1-2.

NELLCOR™ Oximax Sensors™, Tyco Healthcare Group, 2002, pp. 1-5.

Nellcor Oximax, Sensor Selection Guide, Tyco Healthcare, Oct. 2002, 12 pages.

(56)

References Cited

OTHER PUBLICATIONS

Principal of Operation (viscosity measurement), Norcross Corporation, http://www.viscosity.com/faq_poo.asp, downloaded Nov. 8, 2007, 1 page.
U.S. Appl. No. 11/314,545, filed Dec. 20, 2005.
U.S. Appl. No. 11/888,723, filed Sep. 2, 2007.
U.S. Appl. No. 11/821,150, filed Jun. 22, 2007.
Third Office Action for CN Patent Application No. 200610150484.7, dated Dec. 6, 2010.

Notice of Grant of Patent Right for CN Patent Application No. 200610150494.7, dated Jun. 30, 2011.

First Office Action for CN Patent Application No. 200810150494.7, dated Nov. 27, 2009 (9 pages).

Second Office Action for CN Patent Application No. 200610150494.7, dated Sep. 3, 2010 (11 pages).

Sorbero et al. Assessment of Pay-for-Performance Options for Medicare Physician Services: Final Report. RAND Health. May 2006.

* cited by examiner

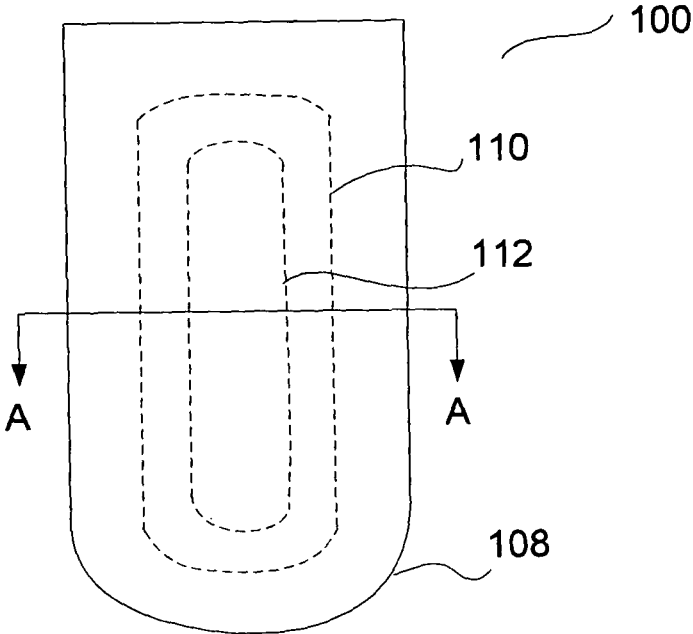


Fig. 1A

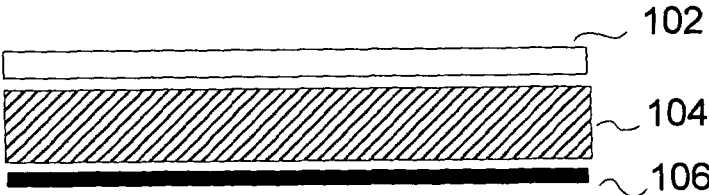


Fig. 1B

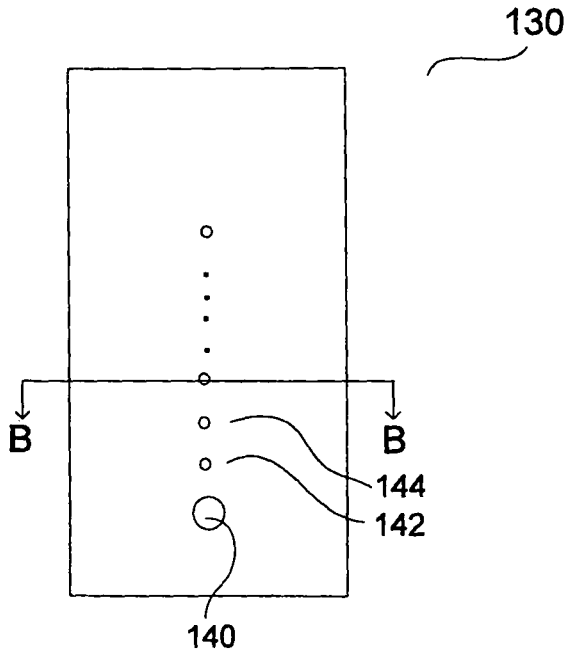


Fig. 1C

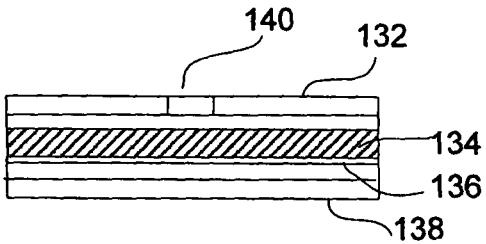


Fig. 1D

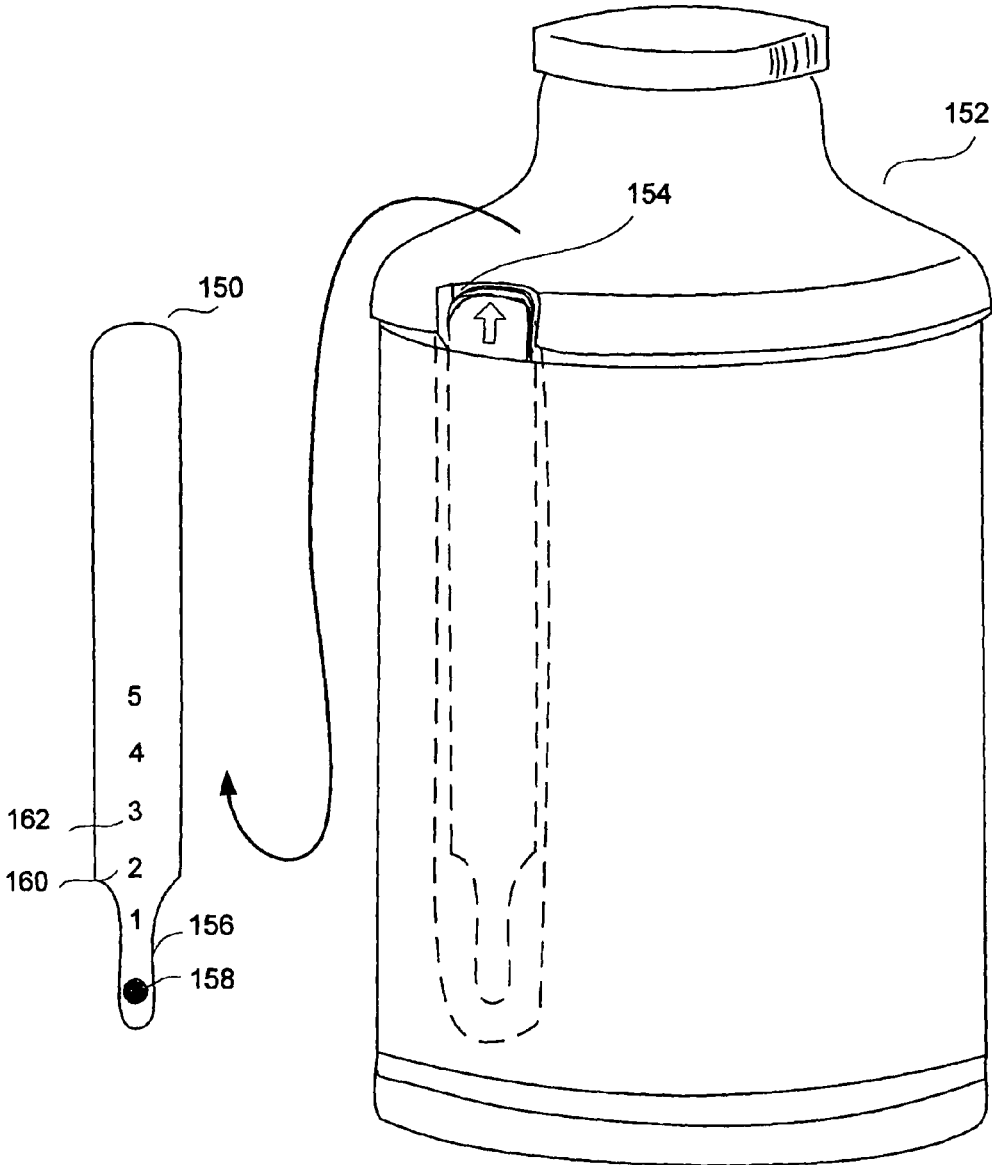


Fig. 2

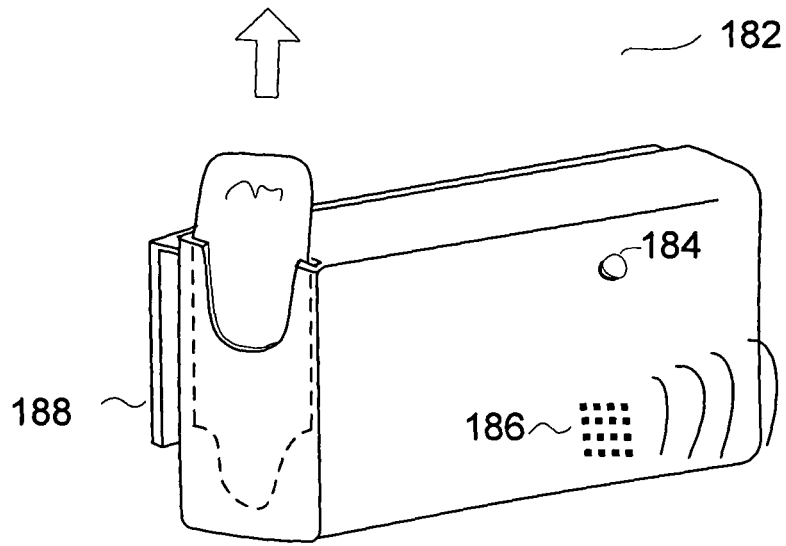


Fig. 3B

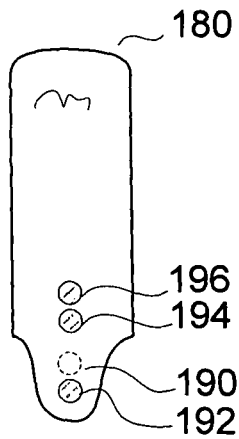


Fig. 3A

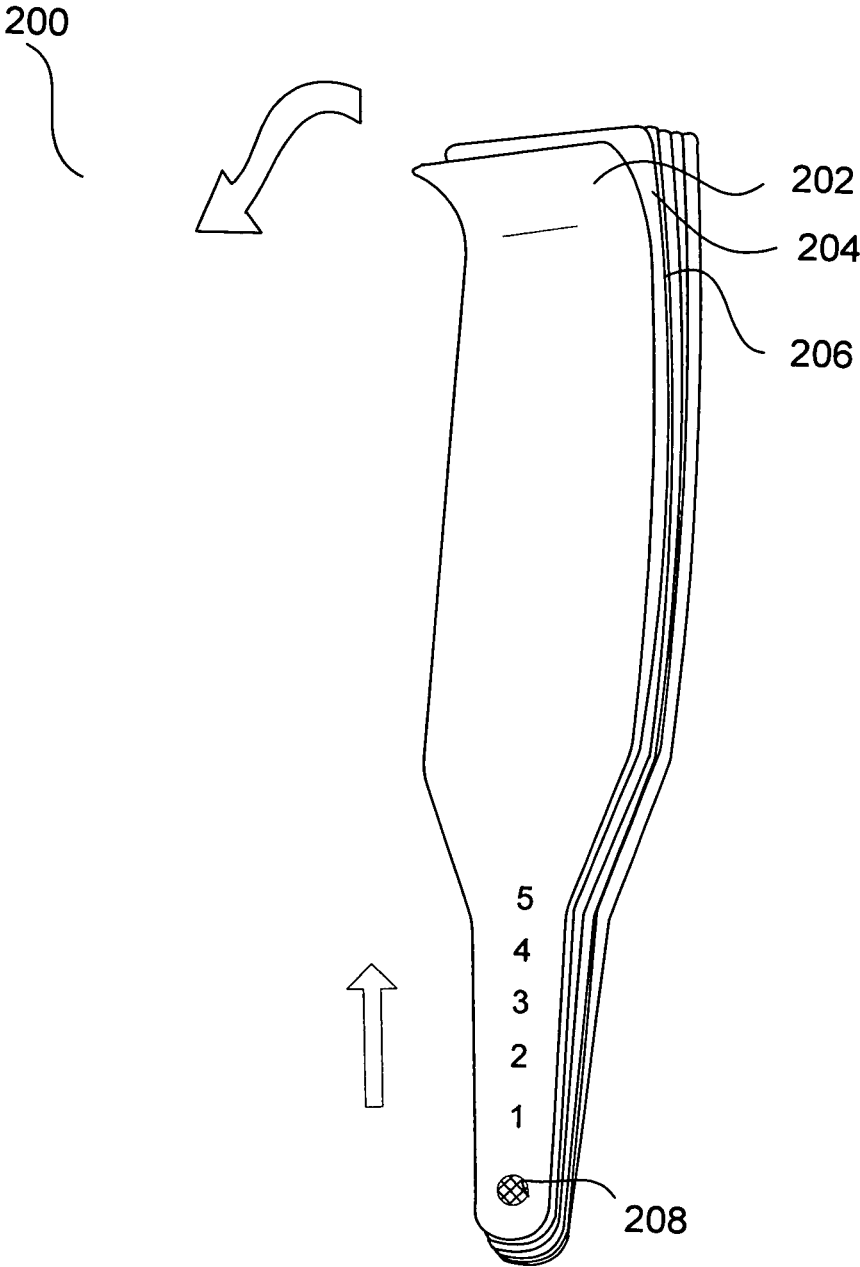


Fig. 4

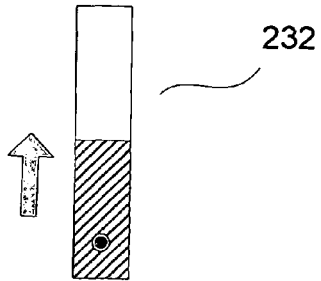


Fig. 5B

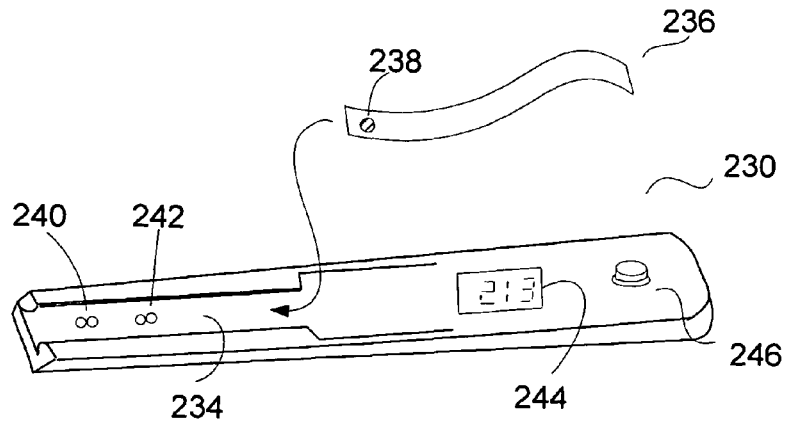
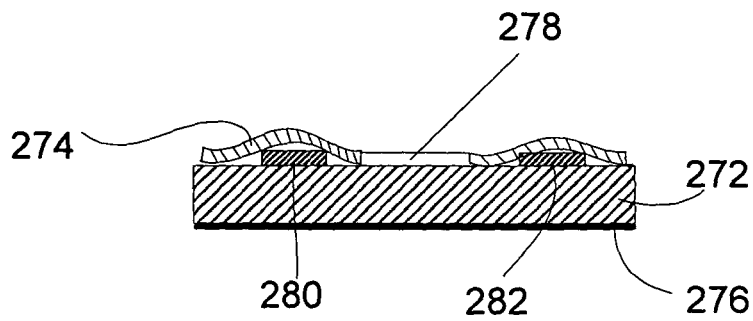
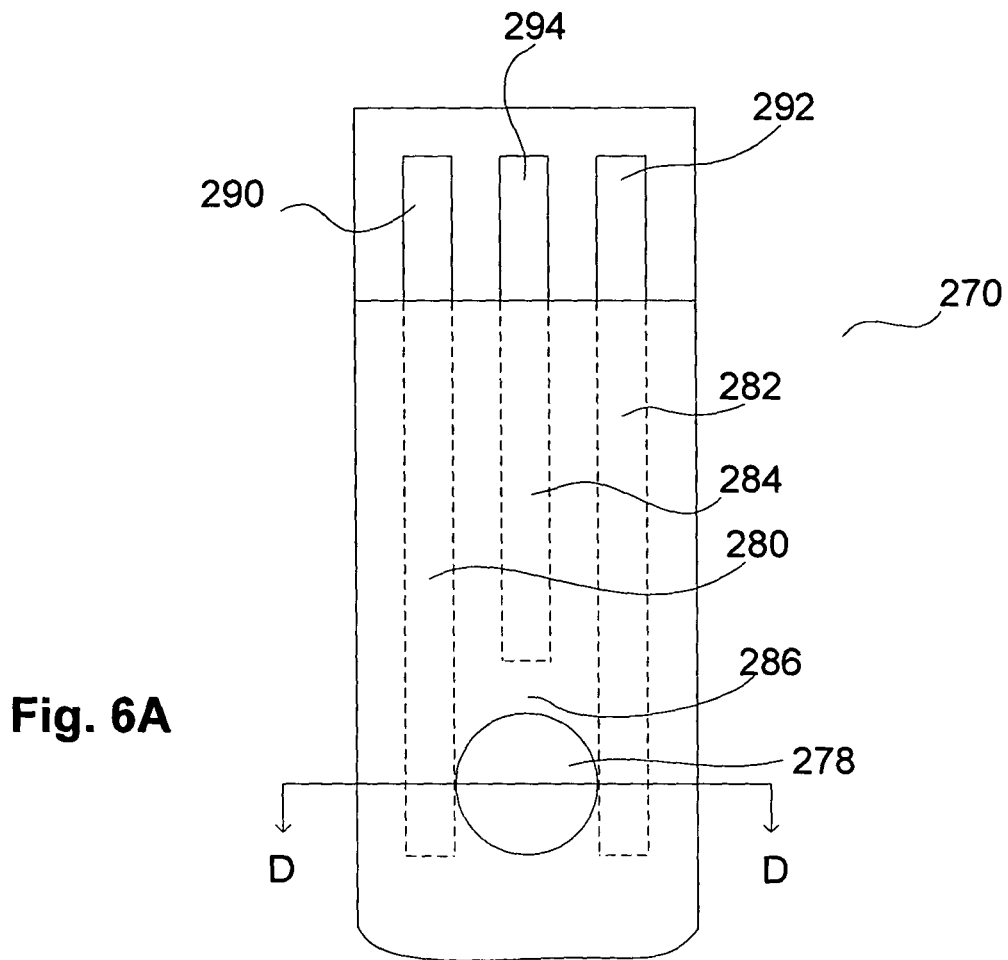


Fig. 5A



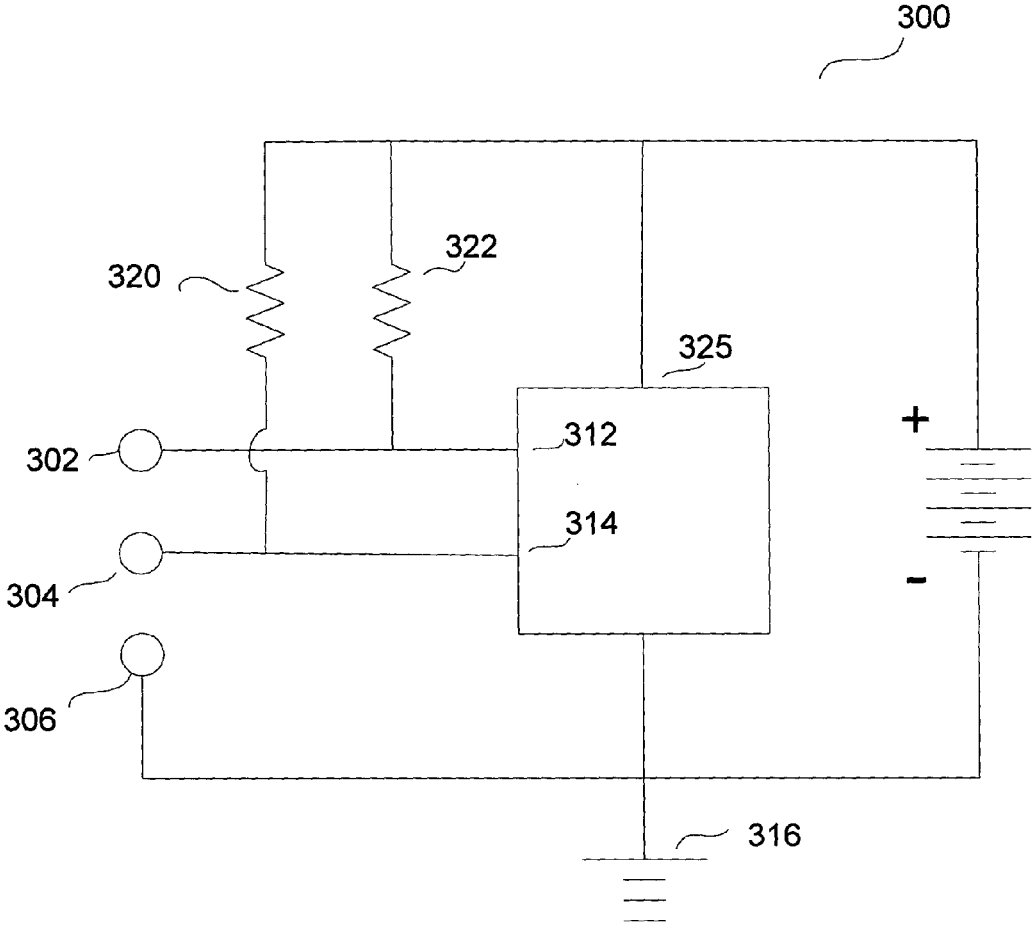


Fig. 7A

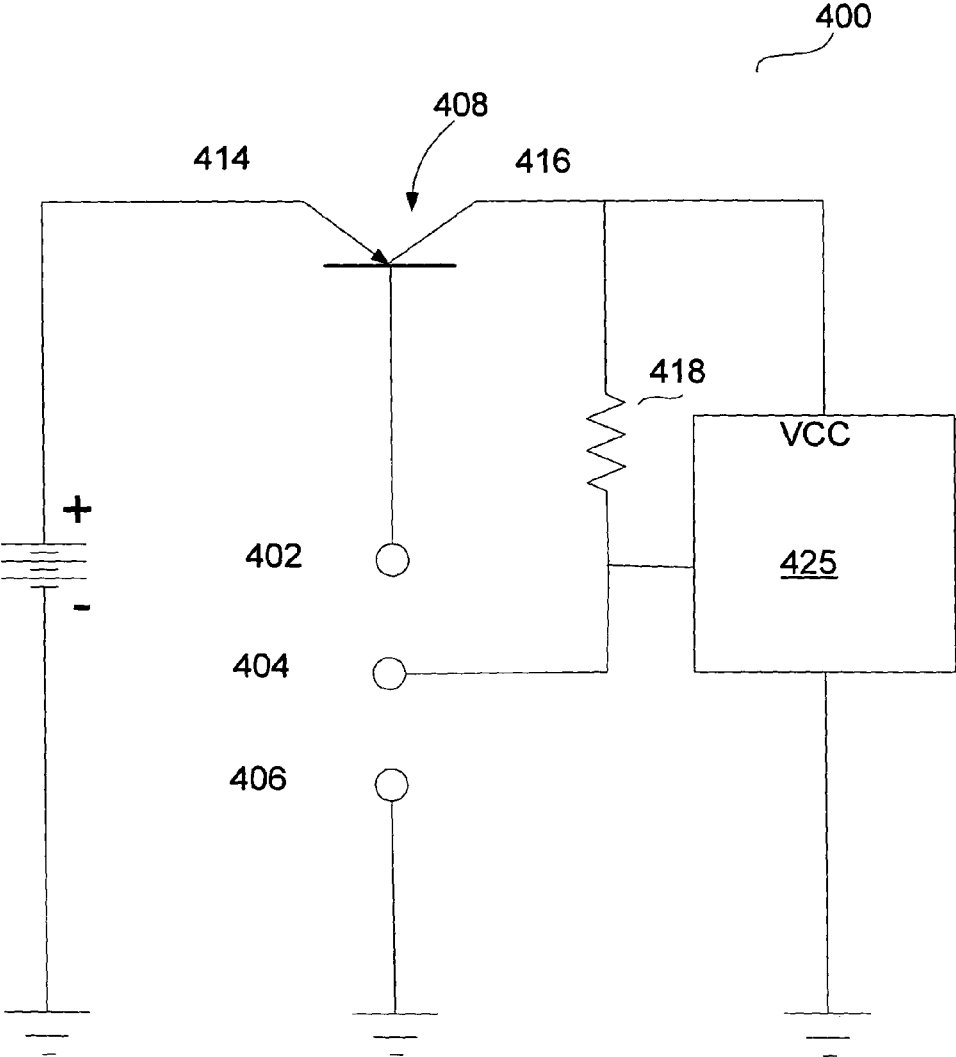


Fig. 7B

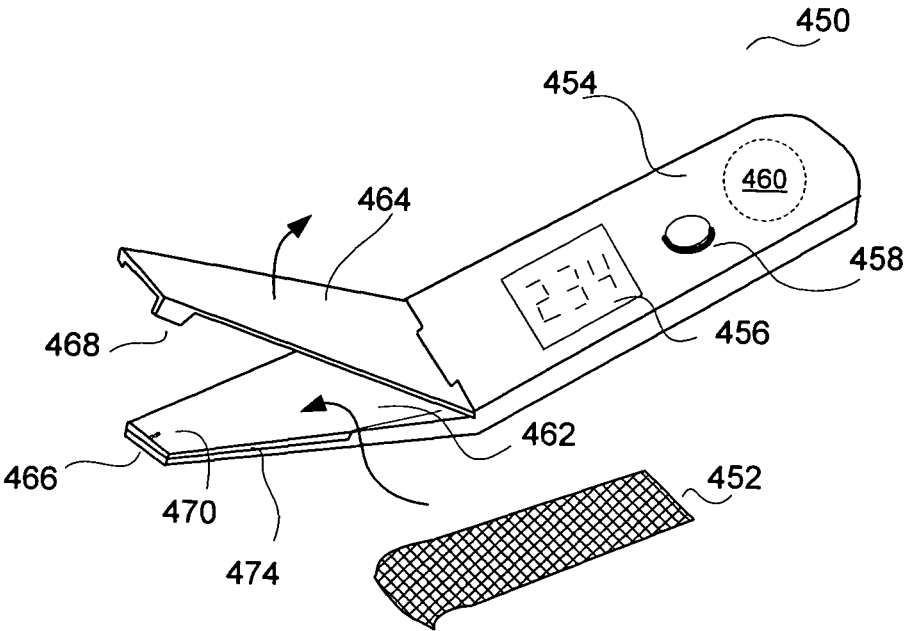


Fig. 8A

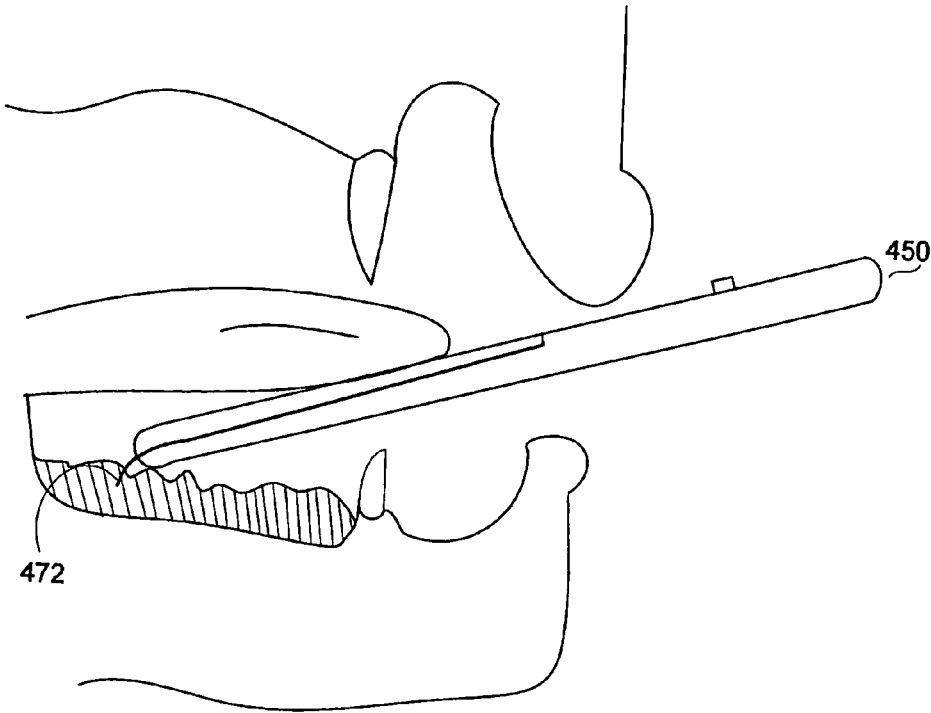


Fig. 8B

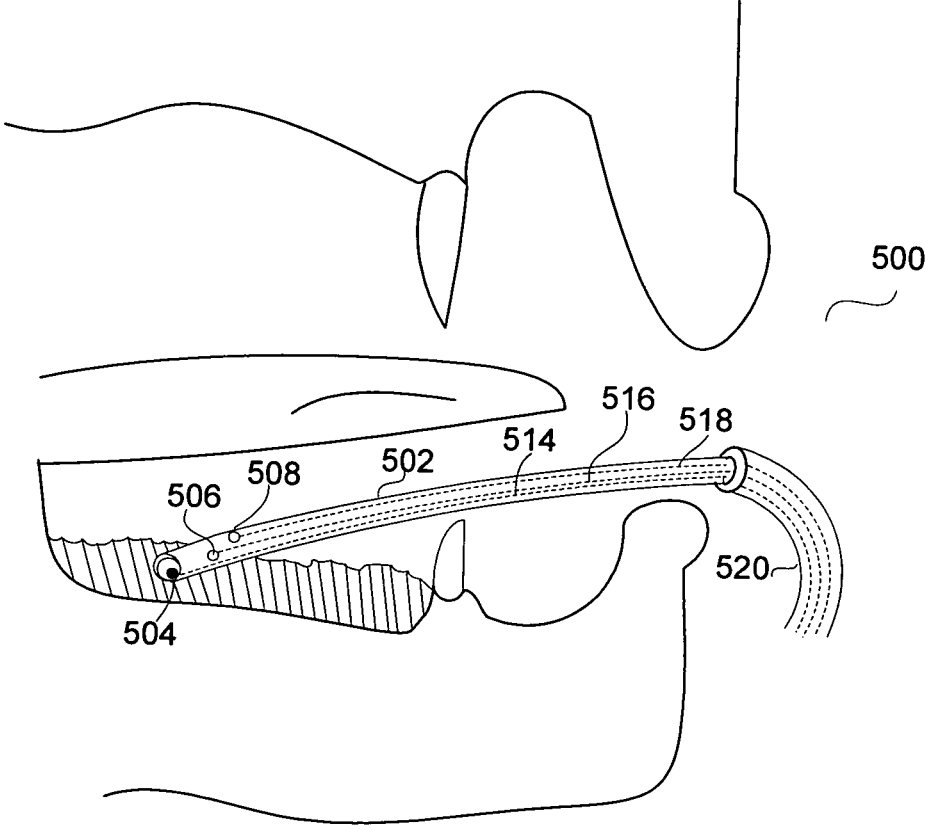


Fig. 9

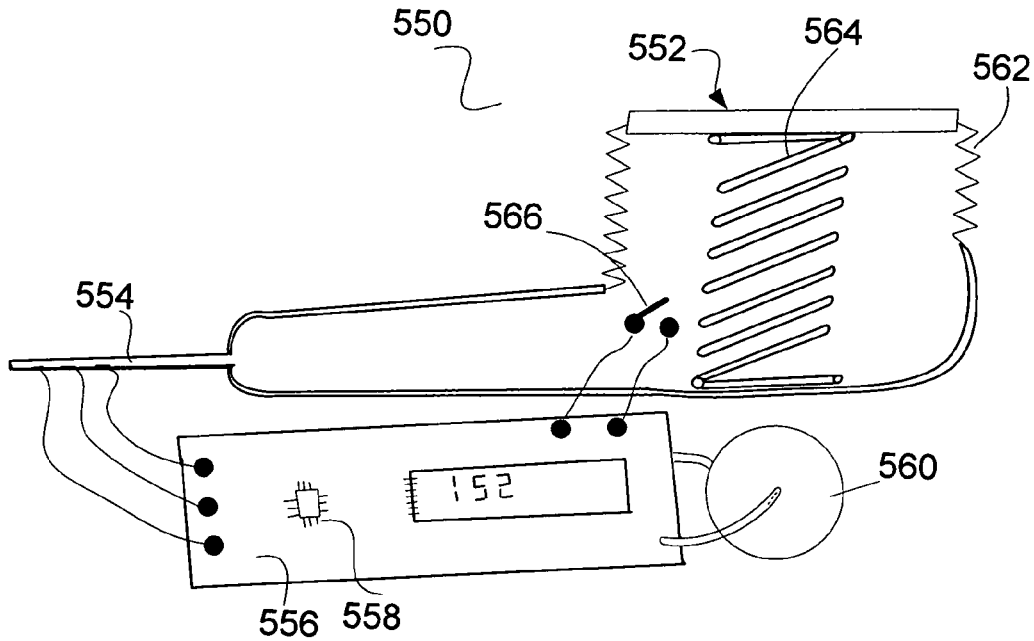


Fig. 10B

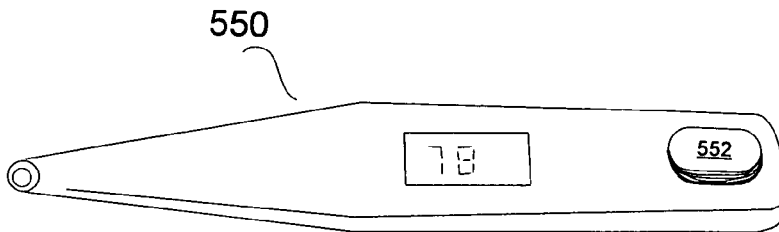


Fig. 10A

Fig. 11A

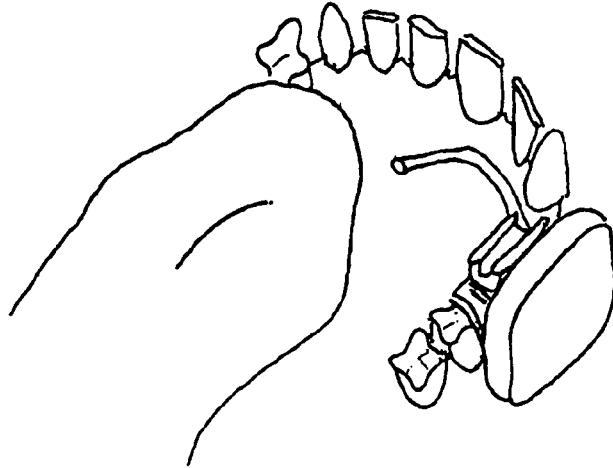


Fig. 11B

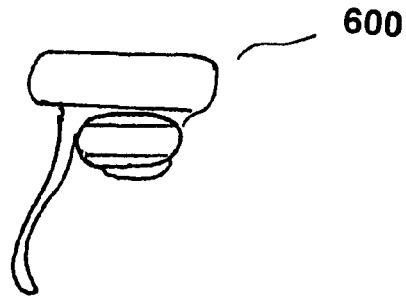
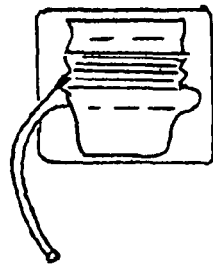
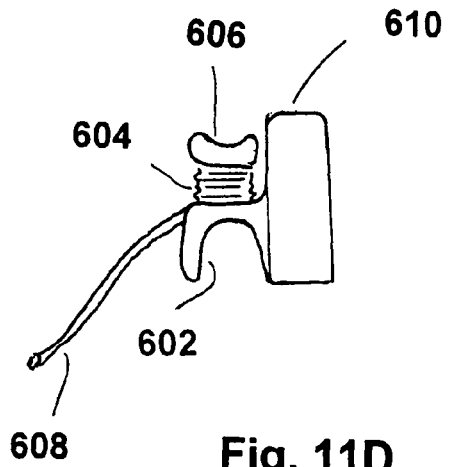


Fig. 11C



608

Fig. 11D



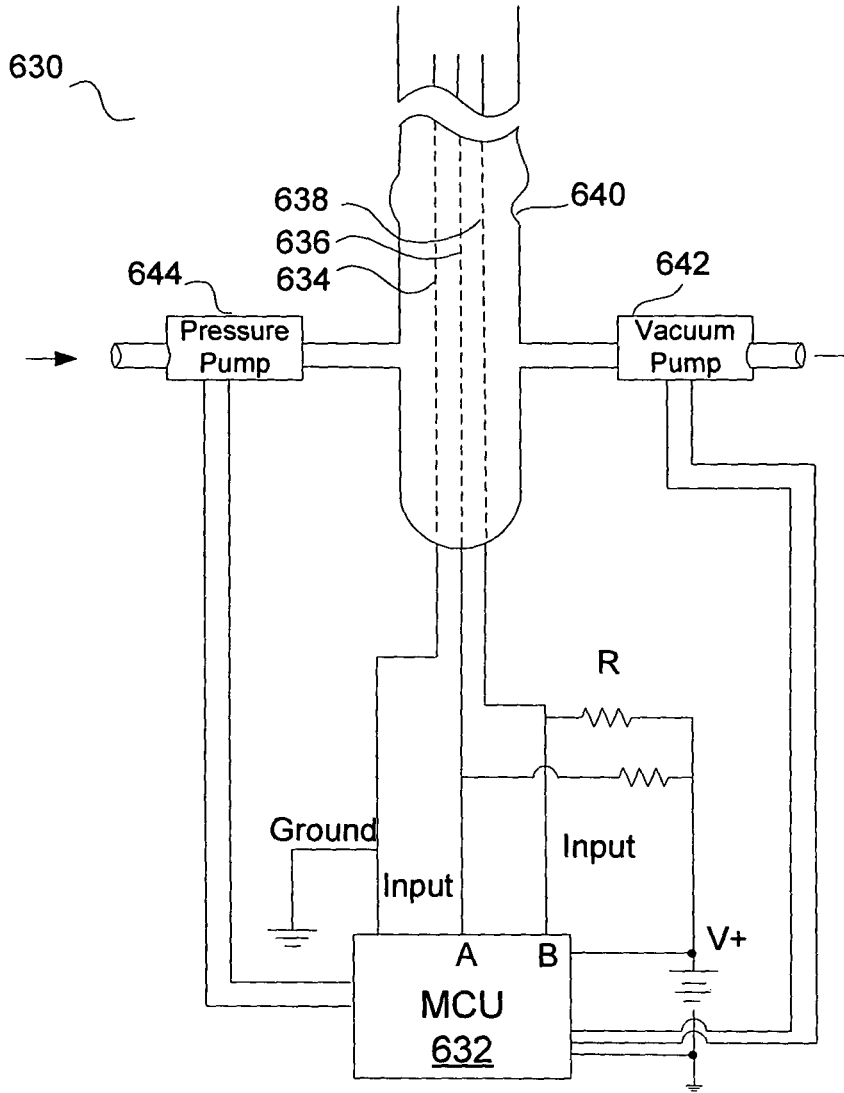


Fig. 12

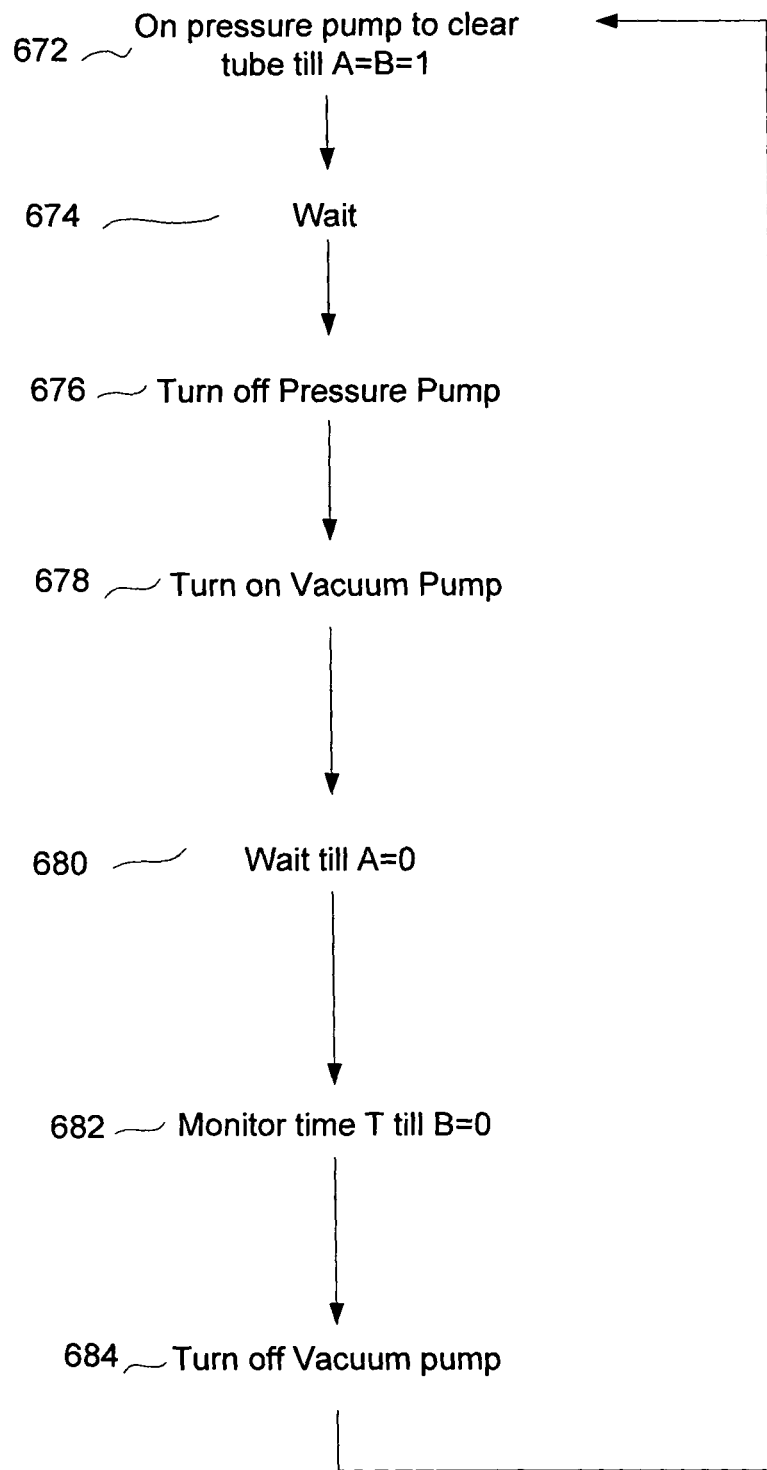


Fig. 13

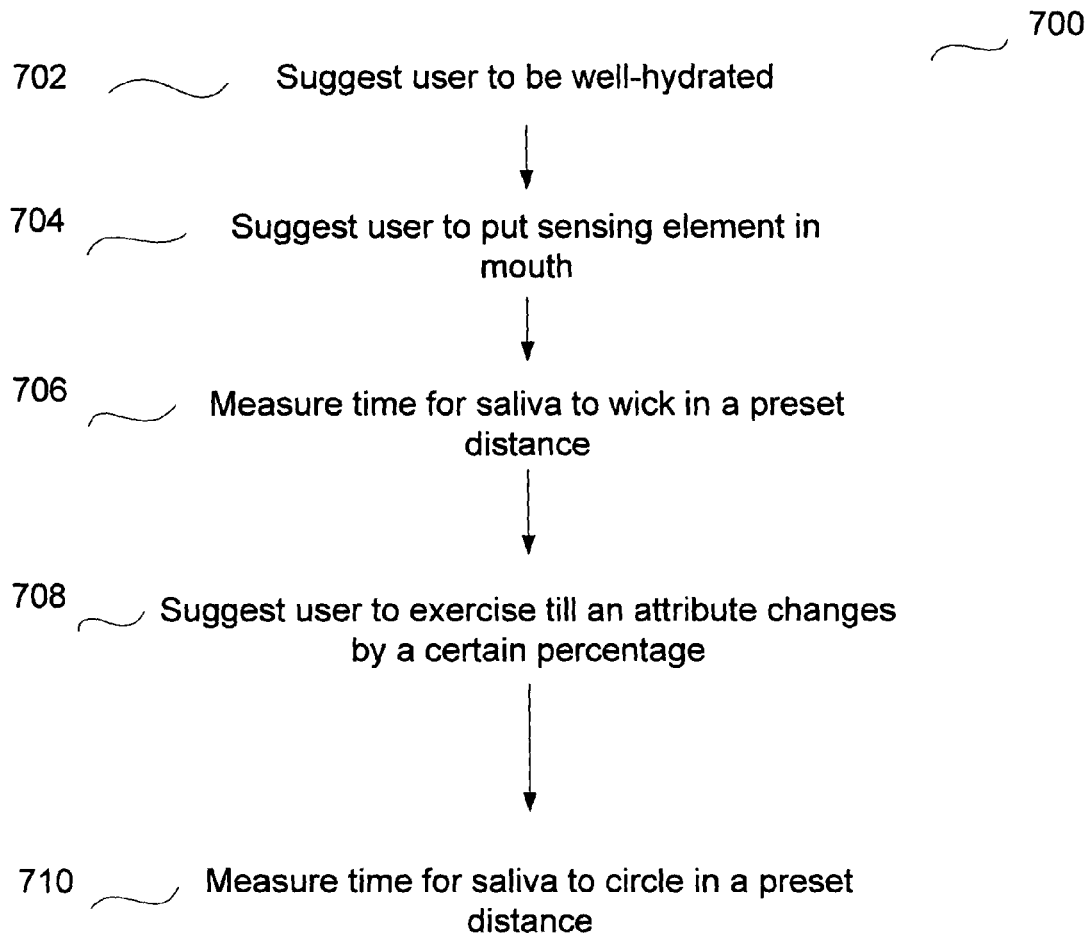


Fig. 14

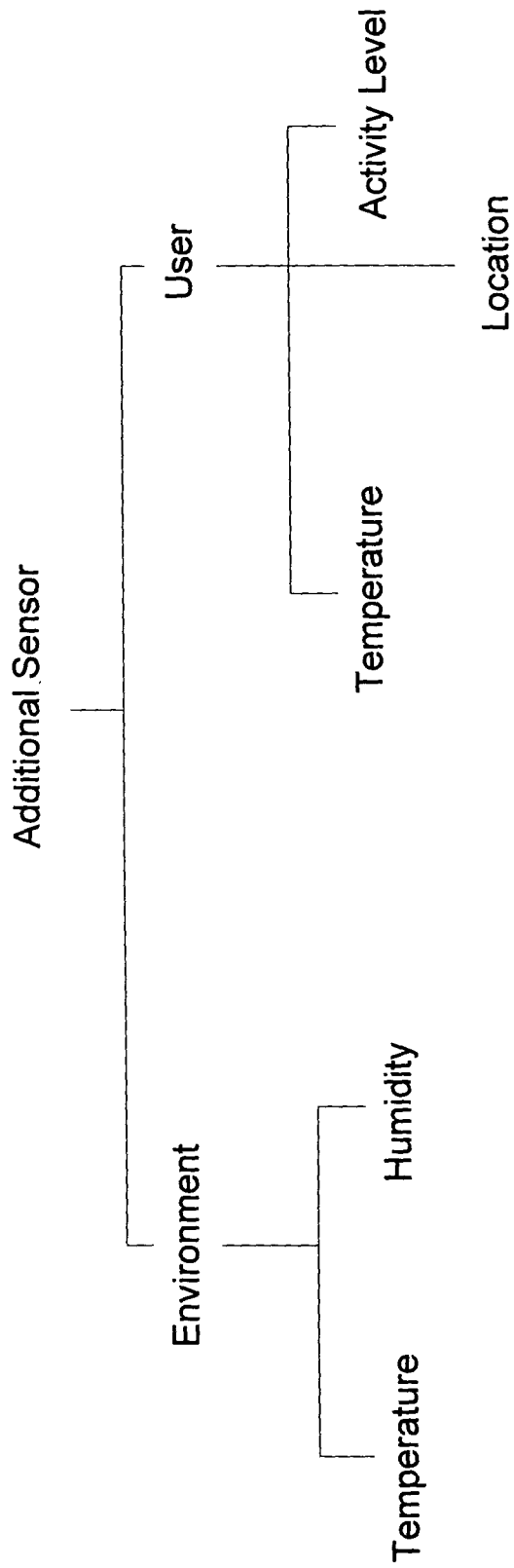


Fig. 15

1

METHOD AND APPARATUS TO SENSE HYDRATION LEVEL OF A PERSON

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is related to U.S. patent application Ser. No. 11/314,545, filed Dec. 20, 2005, and entitled "BOTTLE OF LOTION WITH A SENSOR," which is hereby incorporated herein by reference, which claims priority to each of: (i) U.S. Provisional Patent Application No. 60/636,969, filed Dec. 20, 2004, entitled "PREVENTIVE MEDICAL SYSTEMS, METHODS AND APPARATUS," and which is hereby incorporated herein by reference; (ii) U.S. Provisional Patent Application No. 60/652,213, filed Feb. 14, 2005, entitled "PREVENTIVE MEDICAL SYSTEMS, METHODS AND APPARATUS," and which is hereby incorporated herein by reference; (iii) U.S. Provisional Patent Application No. 60/670,957, filed Apr. 13, 2005, entitled "BOTTLE OF LOTION WITH A LOTION SENSOR," and which is hereby incorporated herein by reference; (iv) U.S. Provisional Patent Application No. 60/889,312, filed Jun. 10, 2005, entitled "PERSONAL AND PORTABLE BOTTLE," and which is hereby incorporated herein by reference; and (v) U.S. Provisional Patent Application No. 60/732,925, filed Nov. 2, 2005, entitled "METHOD AND APPARATUS TO SENSE HYDRATION LEVEL OF A PERSON," and which is hereby incorporated herein by reference.

This application also claims priority to: (i) U.S. Provisional Patent Application No. 60/732,925, filed Nov. 2, 2005, entitled "METHOD AND APPARATUS TO SENSE HYDRATION LEVEL OF A PERSON," and which is hereby incorporated herein by reference; and (ii) U.S. Provisional Patent Application No. 60/785,825, filed Mar. 24, 2006, entitled "MEDICAL MONITORING SYSTEM," and which is hereby incorporated herein by reference.

In addition, this application is related to: (i) U.S. patent application Ser. No. 11/314,545, filed Dec. 20, 2005, entitled "BOTTLE OF LOTION WITH A SENSOR," and which is hereby incorporated herein by reference; (ii) U.S. patent application Ser. No. 11/451,781, filed Jun. 12, 2006, entitled "PERSONAL AND PORTABLE BOTTLE," and which is hereby incorporated herein by reference; (iii) U.S. patent application Ser. No. 11/451,780, filed Jun. 12, 2006, entitled "HEALTHCARE BASE," and which is hereby incorporated herein by reference; (iv) U.S. patent application Ser. No. 11/479,665, filed Jun. 30, 2006, entitled "MOISTURE SENSOR FOR SKIN," and which is hereby incorporated herein by reference; and (v) U.S. patent application Ser. No. 11/491,774, filed Jul. 22, 2006, entitled "PORTABLE CONTAINER WITH SPEAKER ATTACHED," and which is hereby incorporated herein by reference.

BACKGROUND

In the United States alone, there are more than 30 million adult runners. To maintain proper body temperature, runners sweat. The water in the sweat needs to be replaced. Appropriate hydration is critical for runners, particularly those who are running for a long period of time. Improper hydration is one of the most common reasons why marathon runners require medical attention during races.

Dehydration causes numerous problems. Even being at one-percent dehydration can affect a runner's performance. For example, a one-percent dehydration may lead to a 10% decrease in performance, which can translate to about 1-hour delay over an extended race, such as a triathlon. In other

2

words, a relatively small fluid loss, such as one pint, can decrease athletic performance by 10-15%. In addition to diminished performance, symptoms of dehydration include thirst, irritability, headache, weakness, dizziness, cramps, chills, vomiting, nausea, and head or neck heat sensations.

The severely dehydrated can go into shock and end up losing control of all of their bodily functions. Though terribly thirsty, they cannot drink. Even ice chips in their mouths might make them vomit. At that point, to replenish the lost fluids, they need to have fluids applied intravenously.

Dehydration is not the only problem. Over-hydration can be problematic as well. Runners lose not only water, but also a certain amount of sodium and other minerals while sweating. Runners can consume large quantities of water during their races. This can cause a drop in overall sodium levels and, potentially, hyponatremia, which means low levels of salt in the blood. The problem typically arises when the runner runs for a long duration of time, such as three hours, while drinking only plain water.

The human body plays a delicate balancing act with the concentration of sodium in the blood. Small changes in the balance can be dangerous to a body's osmotic chemistry. Almost every physiological process in our body depends on osmotic gradients, with water moving from an area of lower salt concentration to an area of higher salt concentration. Severe sodium imbalance may lead to seizures, increased intracranial pressure, pulmonary edema (fluid in the lungs), respiratory arrest and even death. Many scientists view hyponatremia being as threatening to runners as dehydration and heat sickness.

To prevent dehydration or over-hydration, one approach is to drink the amount of fluid substantially equal to the sweat and urine losses.

Sometimes thirst may be a good indicator as to when to drink. If you are thirsty, drink. Monitoring the volume and color of urine can be helpful in determining hydration status as well. A general guideline is to drink until your urine is clear. However, by the time you feel thirsty, for example during a workout, you may already be dehydrated. Also, in the heat of a race, a runner may forget or suppress the natural instinct of thirst and not check his urine.

Another approach to determine when to drink is to measure one's body temperature. One recent approach is to swallow a small temperature sensor. However, some athletes may not want to swallow such a foreign object.

One recommendation from a number of marathon associations is to weigh runners prior to a race and again following the race. The drop in weight post-exercise could provide an indication as to roughly how much fluid one needs to replenish. In the heat of a long race, it may not be convenient to weigh oneself during the race. Also, runners must exercise care when stopping to weigh themselves in the middle of a race. Postural hypotension is experienced when a runner suddenly stops. Blood pooling in the legs can lead to inadequate blood supply to other parts of the body. The runner can then feel faint and collapse.

Although running has been used above as an example to illustrate the importance of proper hydration, proper hydration is important in other types of sports, particularly for endurance sports or sports lasting for a long duration of time. The challenges not only fall on the adults, but children as well.

Hydration is also an issue in children. It can be quite difficult to determine whether a toddler is sufficiently hydrated. We cannot depend on whether he is crying or not. He can be distressed for numerous reasons, and the basic reason may not be easily decipherable. The difficulty is exac-

erbedated if the toddler has diarrhea and is vomiting. Typically, particularly for first-time parents, they often take the toddler to a healthcare provider.

It should be apparent from the foregoing that there is a need for ways to determine if a person is appropriately hydrated. Furthermore, it is desirable that the ways be applicable to people of different ages and in different conditions. Also, it would be helpful if at least some of the ways are affordable so that people with limited means can still use them.

SUMMARY

In different embodiments, the present invention provides methods and apparatus to measure the hydration level of a user based on measuring the saliva of the user. The measurements can be used to indicate if the user is appropriately hydrated. Different embodiments are applicable to people of different ages and in different conditions. Some embodiments are inexpensive and disposable. Other embodiments are applicable for more than one-time use. Yet other embodiments are applicable for continual use or re-use.

The invention can be implemented in numerous ways including, a method, system, device, and a computer readable medium. Several embodiments of the invention are discussed below.

In one embodiment, a hydration sensor includes a hydration sensing element. The sensing element can be a disposable sensing element. The sensing element includes a piece of water-permeable material, such as a blotting paper, which can be a piece of filter paper. The blotting paper is sandwiched between two pieces of water-impermeable material. In one example, the water-impermeable materials can be adhesive tapes. To measure the hydration level of a user, the sandwiched blotting paper is placed in the user's mouth. Based on capillary action, saliva gets into the paper from the edges. In one embodiment, the rate at which the saliva flows into the paper is a function of the concentration of water in the saliva, or depends on the viscosity of the saliva. By measuring the extent to which the saliva gets into the paper, the hydration level of the user can be determined.

In one embodiment, the sandwiched blotting paper includes a chemical compound deposited on a first side of the blotting paper. The second side of the paper is exposed to saliva, which diffuses or wicks into the first side. The compound when exposed to saliva or water becomes a conspicuous colored patch. This color patch diffuses back to the second side of the blotting paper. The amount or the extent of the compound that changes color depends on how dehydrated the user is and the duration the paper is in the mouth. For example, if the duration of time is fixed, the amount of the compound that changes color provides an indication on the hydration level of the user.

In one embodiment, the hydration sensing element is a hydration sensor. In another embodiment, the hydration sensing element is incorporated into different apparatus to form a hydration sensor. For example, the element is incorporated to a bottle, which can carry fluid. In another embodiment, the element is incorporated to a carrier, such as a box, which can include a clip to attach the box to the clothing of the user. The box can have a timer. The user can turn on the timer after placing the element into his mouth. After a preset amount of time, the timer will alert the user that the measurement is over and the user can remove the element from his mouth to check for his hydration level. In yet another embodiment, the sensor is a handheld device, which can carry a number of sensing elements.

In one embodiment, a hydration sensor incorporates electrical components to automatically measure a hydration sensing element, such as measure visual indications on the element. For example, the hydration sensor includes photodiodes and photo-sensors to measure the element.

Instead of based on visual indications, in one embodiment, sensing is performed through other electrical means. There can be electrically conducting lines on a piece of water-permeable material, such as blotting paper. The sensor measures the time it takes saliva to diffuse from one electrical line to the next to indicate the hydration level of the user. Instead of on a piece of paper, the conducting lines may be attached to a piece of cloth or a piece of fiberglass cloth. In one embodiment, such sensors are applicable for more than one-time use.

In one embodiment, a hydration sensing element is re-usable, or more adaptable to be used numerous times. For example, the sensing element can include a hollow tube or chamber with a small diameter, with conducting wires inside the tube or chamber. The ends of the wires are staggered relative to the opening of the tube. A timer is used to measure the time it takes for saliva to go from one wire end to another wire end. Based on the time measured, the hydration level of the person can be identified. To re-start measurements, saliva in the tube is cleared. There can be different ways to clear the saliva from the tube. One approach is based on a mechanical air pump.

In another embodiment, a re-usable hydration sensor with a mechanical pump can be made in the shape to fit into the mouth of the user. The mechanical pump is activated by the user biting onto the sensor. The sensor includes a wireless transmitter to send measurements to, for example, a portable device. Based on the measurements received, the portable device can alert the user if he needs to drink.

Instead of a mechanical pump, in one embodiment, the saliva is cleared from the tube with an electro-mechanical pump.

The sensing elements can be made of other types of materials. In one embodiment, the sensing element is a piezoelectric element on an absorbent medium, such as a thin sponge, to measure the viscosity of fluid. The sensor can be used to provide an absolute index of the hydration level of a user.

Different people in different physical and/or environmental condition may need differing amounts of fluid. In one embodiment, a hydration sensor is calibrated. The calibration can be for different types of people in different conditions. A user can perform the calibration. After the calibration, the sensor or that type of sensor can become personalized to the user. For example, before a person starts using a hydration sensor or a type of hydration sensor, the person first gets herself appropriately hydrated. Then, she measures the time it takes for the sensor to indicate that she is appropriately hydrated. The time measured would serve as the base line. Future measurements can be relative to the base line.

An embodiment of a sensor with a wireless transmitter has been described. In one embodiment, the sensor is connected to another device through the wireless transceiver. The connection allows the measured hydration levels to be transmitted to the other device, and allows the sensor to receive signals from the other device, such as recommendation on fluid consumption. The other device can be a portable device also carried by the user, a device not in the vicinity of the user, or a base station in the vicinity of the user. In another embodiment, the sensor is connected to another device through a cable.

Different embodiments regarding packaging the sensor have been described. In other embodiments, the sensor can be incorporated into a spoon or a cup. In another embodiment, a

5

hydration sensor is integrated to a bottle or a container, which can carry fluid or beverages for the user to drink. Some of the electronics in the sensor can be transferred to the bottle or the container. There can be promotional materials or different designs on one or more surfaces of the bottle or the container.

In one embodiment, one or more additional sensors are integrated or coupled to a hydration sensor. The one or more additional sensors are for sensing, for example, a piece of environmental information in the immediate vicinity of the hydration sensor. The additional sensor can be a temperature sensor or a humidity sensor. In another embodiment, an additional sensor can measure another piece of information regarding the person using the hydration sensor, such as the person's body temperature or activity level. The additional sensor information can help determine the appropriate amount of fluid for the user to consume. In another embodiment, the additional sensor information can modify the baseline calibration level of the sensor.

In one embodiment, a hydration sensor also provides recommendation to a person using it. The recommendation can be alerting the person to be aware of other factors that can affect the measurements. For example, an audio signal can tell the person to avoid eating food such as candy immediately before measurements.

Other aspects and advantages of the present invention will become apparent from the following detailed description, which, when taken in conjunction with the accompanying drawings, illustrates by way of example the principles of the invention.

BRIEF DESCRIPTION OF THE DRAWINGS

FIGS. 1A-1D illustrate different embodiments of disposable hydration sensing elements according to the invention.

FIG. 2 illustrates an embodiment of disposable hydration sensing elements coupled to a bottle according to the invention.

FIGS. 3A-3B illustrate an embodiment of a disposable hydration sensing element and its carrier that has a timer according to the invention.

FIG. 4 shows one embodiment of multiple hydration sensing elements in a stack according to the invention.

FIGS. 5A-5B illustrate an embodiment of a handheld hydration sensor that can automatically measure a disposable sensing element according to the invention.

FIGS. 6A-6B illustrate a hydration sensing element applicable for more than one-time use according to an embodiment of the invention.

FIGS. 7A-7B show different embodiments of electrical components to measure the outputs from the sensing element shown, for example, in FIGS. 6A-B, according to the invention.

FIGS. 8A-8B show a hydration sensor applicable for more than one-time use according to an embodiment of the invention.

FIG. 9 shows a re-usable hydration sensing element according to an embodiment of the invention.

FIGS. 10A-10B show an embodiment of a re-usable hydration sensor based on a mechanical pump according to the invention.

FIGS. 11A-11D show a re-usable hydration sensor clipped to the mouth of a user according to one embodiment of the invention.

FIG. 12 shows an embodiment of different electrical components of a re-usable hydration sensor based on an electro-mechanical pump according to the invention.

6

FIG. 13 shows an embodiment of a process for the hydration sensor shown in FIG. 12 according to the invention.

FIG. 14 shows a process to calibrate a hydration sensor according to one embodiment of the invention.

FIG. 15 shows examples of additional sensors applicable for appropriate hydration measurements according to different embodiments of the invention.

Same numerals in FIGS. 1-15 are assigned to similar elements in all the figures. Embodiments of the invention are discussed below with reference to FIGS. 1-15. However, those skilled in the art will readily appreciate that the detailed description given herein with respect to these figures is for explanatory purposes as the invention extends beyond these limited embodiments.

DETAILED DESCRIPTION

In one embodiment, a hydration sensing element measures the hydration level of a user based on measuring the saliva of the user. The sensing element can be configured to measure the viscosity of the saliva of the user. Typically, when the user is well hydrated, his saliva has a higher concentration of water or is less viscous than when he is dehydrated. If the saliva is less viscous, it would wick or move faster or deeper by capillary action into the sensing element. FIGS. 1A-1D illustrate different embodiments of a hydration sensing element more applicable for one-time use.

FIG. 1A shows the top view and FIG. 1B shows a cross-sectional view at AA of one embodiment of a hydration sensing element 100. The element 100 can be a disposable hydration sensor, designed to be used once and then disposed. The element 100 includes a piece of water-permeable material 104, such as blotting paper, sandwiched between two pieces of material, 102 and 106, that are impermeable or substantially impermeable to water. In one embodiment, the water-impermeable material can be adhesive tape. To measure the hydration level of a user, at least a portion of the element 100 is placed in the user's mouth. From at least one of its edges, such as 108, and based on capillary action, saliva diffuses or wicks into the water-permeable material 104. The dryness of the user's mouth, or the characteristics of the user's saliva, determines the amount of saliva getting into, or how far or deep the saliva seeps into, the water-permeable material 104. For example, there can be a number of rings on the paper, such as 110. The user can be considered as well hydrated if within one minute, saliva reaches the inner ring 112 on the paper 104.

In one embodiment, the water-permeable material 104 can be a piece of white filter paper, such as similar to the paper used for coffee filters. In one example, the water-permeable material 104 can be about 4 mils thick. In another example, the water-permeable material 104 can be sandwiched between a piece of translucent (or transparent) tape 102 and a black tape 106. The area where the water-permeable material 104 is wet becomes translucent, allowing the black tape 106 to be seen through the tape 102. As an example, for a normal person, after one minute in his mouth, saliva might extend into the water-permeable material 104 a distance of about 2 millimeters when he is appropriately hydrated. But if the person is dehydrated, saliva might extend in by less than 0.5 millimeter, again after the sensing element is in his mouth for 1 minute.

Instead of seeping in from the edge, in another embodiment, saliva can seep into a sensing element through an opening or hole not at the edge. To illustrate, again the water-permeable material 104 can be sandwiched between two pieces of tape. The edges of the sandwiched water-permeable

material **104** are sealed to prevent saliva from getting in. However, there is a hole or an opening in the middle of one of the tapes. The time it takes for the saliva to extend outward from the middle of the opening can be used to determine the dryness of the mouth.

FIG. 1C shows a top view and FIG. 1D shows a cross-sectional view at BB of another embodiment of a hydration sensing element **130**. The hydration sensing element **130** includes a water-permeable material **134** sandwiched between two water-impermeable materials **132** and **138**. The element **130** can be a disposable hydration sensing element.

In one embodiment, the water-permeable material **134** can be a piece of blotting paper, which again can be a white filter paper. The water-permeable material **134** includes a chemical compound **136** on or coupled to one side, the first side, of the water-permeable material **134**. For example, the chemical compound **136** is deposited on the first side (or a portion of the first side). The two water-impermeable materials again can, for example, be tape. A piece of tape (the first-side tape) **138** covers the compound **136**. The second side of the water-permeable material **134** is also covered by tape (the second-side tape) **132**. In one embodiment, both tapes are not transparent, and can be opaque. The edges of the tapes **132** and **138** are sealed to each other. The second-side tape **132** has an opening **140** that exposes the water-permeable material **134** to saliva. The second-side tape **132** is mostly opaque except having a number of transparent holes **142** and **144** (or spots or circles) at varying distances from the opening. The transparent holes **142** and **144** provide windows to visually see the water-permeable material **134** from the outside. In one embodiment, such as shown in FIG. 1C, the transparent holes **142** and **144** can be arranged in a line from the opening **140**.

In one embodiment, when liquid, such as saliva, touches the water-permeable material **134**, the saliva diffuses or wicks through it to the chemical compound **136** underneath. The part of the chemical compound **136** that gets wet becomes a conspicuous and/or visible color patch, and the visible patch diffuses or wicks through to the second side of the water-permeable material **134**. For example, a colored (e.g., green) patch can appear on the second side. In one implementation, the chemical compound **136** is a water-based paint that is non-toxic and hypoallergenic. When saliva is mixed with the paint, the paint diffuses from the first side to the second side of the water-permeable material **134**. In another example, the chemical compound **136** is a dye, such as a powdered food dye. Again when saliva reaches the dye, the dye diffuses from the first side and shows up on the second side of the paper.

When the sensing element **130** is in the mouth of the user, saliva gets into the opening **140**, goes through the water-permeable material **134** (e.g., white filter paper) and reaches the chemical compound **136**. The chemical compound **136** that is exposed to saliva generates a patch of color, such as a green color on the white filter paper. The green color extends back to the second side of the water-permeable material **134**, or the side with the opening. The number of spots changing color from, such as, white (the color of the paper) to green (the color of the patch) depends on the duration the element **130** is within the mouth and the hydration level of the user. In one embodiment, if one fixes the time the element **130** is to stay in the user's mouth, based on the number of spots that have changed color, the hydration level of the user can be inferred. In another embodiment, the transparent spots are in the shape of alphanumeric symbols, such as numbers. For example, a transparent number closest to the opening **140** can be a numeral one, the second most closest transparent number can

be a numeral two and so on. In other words, for numbers, the numbers can be in a sequence, such as in ascending order, or in descending order.

As described above, in one embodiment, a hydration sensing element includes a piece of water-permeable material with a first side and a second side, a chemical compound coupled to the first side of the water-permeable material, and a first piece and a second piece of water-impermeable material. The chemical compound is located between the first piece of water-impermeable material and the first side of the water-permeable material, while the second piece of water-impermeable material is coupled to the second side of the piece of water-permeable material. In other words, the water-permeable material is located between the two pieces of water-impermeable material. When the hydration sensing element is placed in the mouth of the user, saliva is allowed to reach the water-permeable material and the chemical compound. When saliva is in contact with the chemical compound, the part of the chemical compound that gets wet becomes a visible color patch. At least a portion of one piece of the water-impermeable material is transparent to show at least a portion of the visible color patch. The hydration level of the person is measured depending on the extent of the color patch.

There are different embodiments related to the chemical compound, the water-permeable material and the two pieces of water-impermeable material. These embodiments can be mixed and matched.

One embodiment relates to how saliva reaches the water-permeable material and the compound. In one configuration, at least one edge of the water-permeable material is exposed to allow the saliva to reach the water-permeable material and the compound. In another configuration, there is an opening on either the first or the second piece of water-impermeable material to allow saliva to reach the water-permeable material and the compound.

One embodiment relates to the transparency or the lack of transparency of the two pieces of water-impermeable material. Note that the two pieces can be made of different types of material. In one configuration, one piece of water-impermeable material is transparent. In another configuration, one piece of water-impermeable material is transparent, and the other piece of water-impermeable material is either opaque or translucent. In yet another configuration, the at least a portion of one piece of water-impermeable material that is transparent is in the shape of an alphanumeric symbol.

One embodiment relates to the physical structure or the shape of the chemical compound. In one configuration, the chemical compound is in the shape of a layer or a sheet. The sheet is coupled to the first side of the water-permeable material. In another configuration, the compound is in the form of particles. A number of such particles are at different positions on the first side of the water-permeable material. For example, the compound is a powdered or granular dye. The compound can be food dye, and can be in tiny concentrated grains. With sufficient water, liquid or saliva, the powdered or granular dye can create a conspicuous color patch across at least a portion, which can be a significant portion, of the water-permeable material. In one embodiment the grains deposited at different locations are not of the same color, such as two different colors at two different locations on the water-permeable material.

One embodiment relates to where a color patch is seen. In one configuration, the water-impermeable material with at least a portion being transparent is the second piece of water-impermeable material. At least a portion of a color patch permeates from the first side to the second side of the water-

permeable material to be seen through the second piece of water-impermeable material. In another configuration, the water-impermeable material with at least a portion being transparent is the first piece of water-impermeable material.

In one embodiment, a hydration sensing element is a hydration sensor. In another embodiment, a hydration sensing element is incorporated into different apparatus to form a hydration sensor. For example, a hydration sensing element, such as one shown in FIGS. 1C-1D, can be attached to the end of a small rod or a handle. The hydration sensing element with the handle can become a hydration sensor.

FIG. 2 illustrates one embodiment of disposable hydration sensing elements **150** coupled to a bottle **152** which can carry a type of fluid or beverage. For example, the fluid can be a type of filtered water, electrolyte drinks or sports drinks, such as Gatorade®. The sensing elements **150** can be similar to the element shown in FIGS. 1C-1D. There can be a slot **154** on one side of the bottle **152** to carry the sensing elements **150**. Each sensing element **150** can have a narrower section **156**, which is the section to be put in the mouth of the user. An opening **158** can be provided close to the end of the narrower section **156** to receive saliva. Windows, **160** and **162**, to the water-permeable material (e.g., filter paper) can be numbers, instead of just holes. Based on the measurement, one or more of such numbers can change color. For example, if only the numeral “1” changes color, the user is rather dehydrated so she should drink some fluid.

In another embodiment, sensing elements are stored in or carried by a carrier. The sensing elements with the carrier can be a hydration sensor. FIG. 3A illustrates an embodiment of a disposable hydration sensing element **180**. FIG. 3B illustrates an embodiment of a carrier **182** that has, among other components, a timer, a switch **184** (such as an activation switch), an audio device **186** and a power source, such as a battery or a solar cell.

The carrier **182** shown in FIG. 3B can hold a number of the hydration sensing elements **180**. In this example, the carrier **182** can be a handheld or wearable electronic device. In one embodiment, the carrier **182** can be in the shape of a box. The carrier **182** can have a mechanical device **188**, such as a clip, to clamp or attach the carrier **182** onto the clothing of a user. In another embodiment, the carrier **182** can be configured into a wrist band and is carried on the wrist of the user, just like a watch. In yet another embodiment, the carrier **182** also functions as a watch and can include a display. In still another embodiment, the carrier **182** can be incorporated in or attached to a piece of clothing (e.g., helmet, hat, vest, belt, or shirt) of the user, or incorporate in or attach to a portable electronic device carried or worn by the user.

The sensing element **180** shown in FIG. 3A can be similar to the elements shown in FIG. 2 or the element shown in FIGS. 1C-1D. For example, the element **180** can have a piece of water-permeable material (e.g., blotting paper) laminated between two pieces of tape. In this embodiment, the compound that produces color patches is on the same surface of the water-permeable material as the surface that is exposed to the opening. In this embodiment, there are a number of dots of a compound, and they can be of different color and at different distances from the opening **190**. When they are not wet, the compound is a very small amount of dry powder and is inconspicuous. These can be grains of powder food dye. The grains can be of different color, such as red, blue and green. When there is liquid, the dye dissolves and a color patch is formed. In FIG. 3A, there are three dots. The dot nearest **192** to the opening **190** can be red in color; the second closest **194** can be blue and the furthest away **196** can be green.

To measure hydration level, the user pulls one of the sensing elements **180** out from the carrier **182**, places at least a portion of the element **180** in his mouth and then pushes the button or switch **184** on the carrier **182**. This will activate the timer. After a duration of time, such as 1 minute, the timer will activate the audio device **186**, such as a beeper, which would beep. This will alert the user to remove the element **180** from his mouth and read it. If only the red dot **192** shows up, the user is very dehydrated. If a red **192** and a blue **194** dots show up, then the user is mildly dehydrated. If all three dots can be seen, the user is well hydrated.

FIG. 4 shows one embodiment **200** of multiple hydration sensing elements **202** and **204** linked, attached or stuck together into a stack. Each element, such as **202** and **204**, can be similar to the element **150** shown in FIG. 2. In one embodiment, the elements **202** and **204** are glued or connected together, such as at their edges, **206**. For example, this connection at the edges could provide a waterproof seal. To use each element, the user can peel one off and put it in his mouth. Alternatively, in one embodiment, the user can put the entire stack into his mouth. Saliva only goes into the top element because the only opening exposed is the opening **208** of the top element **202**. After the measurement, the user can peel off the top element **202**, and the opening in the next element, the element **204** beneath the top element **202**, is exposed to be used.

FIG. 5A illustrates an embodiment of a handheld hydration sensor **230** that can measure a sensing element. In one embodiment, the handheld hydration sensor **230** can measure a sensing element **232** such as shown in FIG. 5B.

The sensing element **232** shown in FIG. 5B can be similar to the one shown in FIG. 4, except that the water-impermeable material with the opening for saliva to get to the water-permeable material can be transparent. To take a measurement, the user places one such sensing element **236** into a slot **234** on top of the handheld hydration sensor **230**. Next, the user places at least a portion (such as the narrower end) of the sensor **230** into his mouth, under his tongue, like a thermometer. The saliva in the user's mouth will permeate or wick from the opening **238** up the length of the sensing element **236**, causing a color change to move up the sensing element as shown, for example, by the arrow in FIG. 5B. As shown in FIG. 5A, in the slot **234** of the handheld hydration sensor **230** there are two LED/photodiode pairs, **240** and **242**, that sense the color change of the element.

Though there can be many pairs of photodiodes and photo-detectors along the slot **234**, only two are shown. Each photodiode and photo-detector pair measures color change at different distance away from the opening, with the diode emitting light and the corresponding detector measuring the reflected radiation. In one embodiment, based on measuring changes in the reflected light from the different detectors, the extent that the saliva has diffused into the sensing element can be identified.

The handheld hydration sensor **230** in FIG. 5A can also include a timer **244** and a switch, such as an activation switch, **246**, which can be functionally similar to the timer and switch shown in FIG. 3B. In one embodiment, the handheld hydration sensor **230** can include at least two pairs of LED/photo-detector positioned at different position in the slot **234**, such as described above. The timer can track the time it takes saliva to wick up the element from the position of the first pair to the second pair. With the distance between the two pairs known, the handheld hydration sensor **230** can measure the rate the compound changes color, or the speed the color moves up the element.

11

A number of embodiments of hydration sensing elements have been described. They are typically based on visual measurements. They are typically more applicable for single use and can be disposable.

In one embodiment, a hydration sensing element uses electrical resistive measurements. The sensing element can be applicable for more than one-time use. FIGS. 6A-6B illustrate an embodiment of such a hydration sensing element 270. FIG. 6A shows the top view of the hydration sensing element 270, and FIG. 6B a cross sectional view at DD. In one such embodiment, the sensing element 270 includes a piece of water-permeable material 272, such as a piece of blotter paper, sandwiched between two pieces of water-impermeable material 274 and 276. The two pieces of water-impermeable material 274 and 276 do not have to be transparent, and they can be tape 274 and 276. The top piece of tape 274 includes an opening 278, exposing a small part of the piece of the water-permeable material 272. There are a number of electrically conducting lines on the water-permeable material 272. In one embodiment, there are two conducting lines, such as the two outer lines, 280 and 282, shown in FIG. 6A. They are covered or encapsulated by the top piece of water-impermeable material 274. Each of the lines 280 and 282 has its corresponding metal contacts, such as the left conducting line 280 has a left contact 290 and the right conducting line 282 has a right contact 292.

A user can place the sensing element 270 shown in FIG. 6A in his mouth. Saliva then goes through the opening 278 and is absorbed by the water-permeable material 272. With saliva in the opening 278, the resistance between the lines, such as lines 280 and 282, is reduced. By measuring the resistance between the lines, one can determine how wet/dry the mouth is.

The embodiment of the hydration sensing element 270 shown in FIGS. 6A-6B can be coupled to a timer, which can be in a hydration sensor. The timer can be used to measure the resistance change between the conductors as a function of time after a sensing element is placed in the mouth. For example, before the user puts the sensing element in his mouth, the user activates the timer. At that point, the water-permeable material is dry, and the resistance between the lines can be in the range of more than 10 mega-ohms. The timer starts counting after it is activated (i.e., turned on). In one embodiment, the timer can stop counting when the resistance between the lines drops below a preset threshold, for example, 1 mega-ohm. The timer records the time elapsed. In one embodiment, the timer can produce a beeping sound or a flashing LED to indicate to the user that the resistance has dropped to the preset threshold, and the hydration measurement has been completed. The user can then take the sensing element out of his mouth, and the hydration level of the user can depend on the elapsed time. In another embodiment, the elapsed time can be preset to measure the resistance between the lines. The hydration level can depend on the resistance value.

In yet another embodiment, referring to FIG. 6A, the hydration sensing element 270 includes a mechanism to initiate measuring the hydration level of the user. In this embodiment, there is a third conducting line 284 between the two outer lines 280 and 282. This third line 284 can have its own contact 294. In one embodiment, at least a portion of each of the outer electrically-conducting lines 280 and 282 is closer to the opening 278 than the third conducting line 284. For example, a small portion of the edges of the outer two conducting lines 280 and 282 are exposed to the opening, and the third conducting line 284 is recessed at a certain distance 286 from the opening 278. When the user puts the sensing element

12

270 into his mouth, the saliva can reduce the resistance between the outer two conducting lines 280 and 282 almost immediately. For example, a timer can start counting when the resistance between the outside lines 280 and 282 drops below a preset value. In other words, when the resistance between the two outer conducting lines is below a preset value, the sensing element 270 starts sensing the hydration level of the user. Then, as saliva continues to diffuse into the water-permeable material 272, the resistance between the middle contact 294 and the contacts of either or both of the outer conducting lines 290 and 292 drops. Again, in one embodiment, when this resistance drops, which can be below a certain preset value, the timer stops counting.

As discussed, the water-permeable material 272 shown in FIG. 6A can be based on a piece of paper, such as blotting paper. In another embodiment, the water-permeable material 272 is a piece of cloth, such as polyester cloth. The conducting wires can be glued, sewn or integrated into the water-permeable material, such as cloth, or they can be printed with electrically conductive ink onto the material.

In another embodiment, instead of sandwiched between water-impermeable materials, like tape, the water-permeable material can be encapsulated, pressed or heat-sealed in between two pieces of harder and/or more durable materials, such as plastic strips or printed circuit boards. The strips or boards have their corresponding openings for saliva to get in. In one embodiment, the conducting wires can be on one of the strips or boards, which are coupled to or pressed against the water-permeable material, such as cloth or paper.

The hydration sensing element 270 shown in FIG. 6A can be applicable for more than one-time use. One approach is to let the sensing element 270 dry after it has been in the mouth of the user. When it is dry, the user can use the sensing element 270 again for measurement. Alternatively, the user can dip the sensing element 270 in rubbing alcohol, which would speed up the drying process and disinfect the sensing element 270. If the water-permeable material is a piece of cloth, in one embodiment, the user can more easily wash and dry it after it is used.

In one embodiment, a small amount of salt (or other types of resistance-lowering materials) is added in the water-permeable material shown in FIG. 6A, such as in between or among the lines. The resistance-lowering materials can be used to reduce the resistance measured when there is fluid, such as saliva, in between the lines.

FIG. 7A shows an embodiment 300 of electrical components to measure the outputs from a sensing element, such as the sensing element 270 shown, for example, in FIGS. 6A-6B. In FIG. 7A, the three contacts, 290, 294 and 292 from the sensing element 270 shown in FIG. 6A are connected to a first input terminal 302 and a second input terminal 304 of a microcontroller unit 325 and to a ground input terminal 306, respectively. Two inputs 312 and 314 of the microcontroller unit 325 are connected to the first terminal input 302 and the second terminal input 304, respectively. In addition, the two inputs 312 and 314 are also connected to the Vcc of the microcontroller unit 325 through two resistors 320 and 322. The two resistors 320 and 322 can, for example, be 10 mega-ohm resistors. A battery is connected between Vcc and ground 316. The microcontroller unit 325 can include a counter and is programmed so that when an input signal that is lower than a first threshold value is registered between the first input terminal 302 and ground 316, the counter starts counting. This occurs when the resistance between the outer contacts 290 and 292 of the sensing element 270 drops lower than the first threshold value. The time interval between counts can be fixed. The counter stops counting when an input

signal that is lower than a second threshold value is registered between the second input terminal 304 and ground 316. The number of counts is registered. As an example, assume the battery is 1.5 volts, the first threshold value is 0.75 volts and the second threshold value is also 0.75 volts. The microcontroller unit 325 can also be programmed to convert the count to a dryness level, and display the dryness level on a display. To convert the count to a dryness level, there can be a conversion table stored in the unit 325. For example, one approach can be that a count number within a certain range implies that the user is well hydrated. Such a conversion table can be determined based on calibrating the sensing element, which is further discussed below.

FIG. 7B shows another embodiment 400 of sensor electronics applicable for a hydration sensing element, such as the sensing element 270 shown, for example, in FIGS. 6A-6B. In this embodiment, the three contacts 290, 294 and 292 from the sensing element 270 shown in FIG. 6A are connected to the base 402 of a PNP transistor 408, an input pin 404 of a microcontroller 425, and ground 406 respectively. A battery is connected to the emitter 414 of the transistor 408 and to ground 406. A resistor 418 is connected between the input pin 404 of the controller 425 and to the collector 416 of the transistor 408, which is connected to the positive power-supply (VCC) input of the microcontroller unit 425. To illustrate, in one embodiment, the battery is 1.5 volts, and the resistor 418 is 10 mega-ohms. When the voltage between the outer contacts shown in FIG. 6A (or the voltage at the base of the transistor) reaches, for example, 0.7 volts, the transistor 408 starts to conduct, connecting the positive terminal of the battery to the VCC input of the microcontroller unit 425. This would turn on the microcontroller unit 425, and the microcontroller unit 425 would be programmed to start counting. The middle contact 294 of the sensing element 270 is connected to the collector 416 of the transistor 408 through the resistor 418. When the input at the input pin 404 of the microcontroller unit 425 reaches, for example, 0.75 volts, the unit 425 is programmed to stop counting. Again, the number of counts can be converted by the microcontroller unit 425 to a hydration level, and can be displayed.

FIGS. 8A-8B show an embodiment of a hydration sensor 450 that is applicable for more than one-time use. FIG. 8A shows a hydration sensor housing 454 for the sensor 450. The sensor housing 454 includes a timer 456 (which can also function as a clock), a switch 458, such as an on/off switch, and a power source 460, such as a battery, among other electronics. The front portion of the housing 454 includes a cavity 462, which can be closed by a hinged door 464. In one embodiment, the door 464 can be locked by a clip 468 at the tip of the door 464. When the door 464 is closed, the door 464 encloses the cavity 462, except that at least one end 466 (a first end) of the cavity is not fully closed.

The cavity 462 can hold a sensing element, which, in one embodiment, is a piece of water permeable material 452. The water-permeable material 452 can, for example, be a blotting paper, or a piece of cloth, such as fiberglass cloth or polyester cloth.

In one embodiment, inside the cavity 462 there are a number of electrical contacts 470, such as three contacts, and they are positioned proximate to the first end 466 of the sensor housing 454. In one embodiment, the contacts 470 can be on the surface of a printed circuit board in the cavity 462.

The hydration sensor 450 shown in FIG. 8A can be used to measure the user's hydration level. Assume that there are a number of electrical contacts 470, such as three contacts. The contacts 470 are spaced apart, with the resistance value between the first two contacts from the first end 466 of the

sensor housing 454 for starting the timer 456, and with the resistance value between the second and the third contacts for stopping the timer 456. The spacing between any two contacts can be, for example, 0.010 inches. The three contacts can be the three contacts for the circuits shown in FIG. 7A, with the first contact from the first end 466 being a ground contact, the second and third contacts going to the controller. Alternatively, the three contacts can be for the circuits shown in FIG. 7B, with the first contact being ground, the second being the contact to the base of the transistor and the third being the contact to the input of the controller.

To measure hydration level, a sensing element, such as 452, is placed inside the cavity 462, with the door 464 closed, but with a small portion of the sensing element 452 exposed from the first end 466 of the hydration sensor 450. The sensing element 452 is touching the contacts 470; this can be done by having the closed door 464 pushing the element 452 to couple to the contacts. As shown in FIG. 8B, the user inserts the hydration sensor 450 under his tongue and pushes the switch 458 to activate the sensor 450, which can activate the timer 456. The saliva from the user touches the exposed portion 472 of the sensing element 452 and wicks up into the sensing element 452. When the saliva lowers the resistance between the first and the second contacts from the first end 466 to a first preset value, the timer 456 starts counting. When the saliva lowers the resistance between the second and the third contacts from the first end 466 to a second preset value (which can be the same as the first preset value), the timer 456 stops counting. The time elapsed or the number of counts provides an indication to the hydration level of the user.

In one embodiment, to improve the electrical connection between the sensing element 452 and the contacts 470 in the sensor housing, there is an elastomer or a small spring under the door 464 in the vicinity of the contacts 470. When the door 464 is closed, the elastomer or spring presses the sensing element 462 against the contacts 470, which enhances or ensures electrical connection between the sensing element 452 and the contacts 470.

In one embodiment, the contacts 470 are close to the first end 466 of the sensor housing 454. They are much closer to the first end 466 than other edges (e.g. 474) of the sensor housing, such as the left and the right edge. This will ensure that the hydration measurement at the contacts is from saliva coming through the first end 466 of the sensor housing, and not from other edges, such as 474.

In one embodiment, the sensing element 452 shown in FIG. 8A is applicable for more than one-time use. For example, the sensing element 452 can be a piece of blotting paper. After it is used, one can allow it to dry and then use it again. In another embodiment, the sensing element 452 is a piece of cloth, such as polyester cloth. After it is used, one can wash the cloth and then use it again.

In one embodiment, there are multiple pieces of the sensing elements 452 in the sensor housing 454. For example, the sensing elements 452 can be provided in a roll. The roll or multiple pieces can be serrated so that after the user has used one piece, the user can pull out that piece (such as from the first end 466 of the sensor housing 454) and remove it at the serrated region. This also brings a new sensing element into position for a next measurement.

A number of embodiments of hydration sensors and sensing elements have been described that are disposable, and a number of embodiments have been described that are applicable for more than one-time use.

In yet another embodiment, the sensing element is reusable. For example, the sensing element can be suitable for continual use. In one embodiment, a re-usable sensing ele-

15

ment includes a small channel (or tube) where capillary action can bring saliva up the channel. In another embodiment, pumping action can also bring saliva up the channel. There are also at least three contacts on the inside of the channel, with, for example, the first two contacts being used to indicate starting of measurements, and, for example, the second and third contacts being used to indicate the end of the measurements. Each contact has its corresponding electrical wire as leads to allow the contacts to be measured. The plurality of contacts are spaced apart up the channel. To determine the hydration level of the user, the channel is positioned inside the mouth of the user, and the resistances between or among the contacts are measured.

FIG. 9 shows an embodiment of a hydration sensing element 500 that is a re-usable type. In this embodiment, the channel of the re-usable sensor is a hollow tube 502 with a small diameter. In one embodiment, because the tube's inner diameter is small, fluid can wick up the tube based on capillary action. In one example, the tube has an inner diameter of about 9 mils. In another example, the tube has an inner diameter of about 5 mils. The tube can be made of different types of materials, such as glass, nylon, polycarbonic and acrylic. In one example, the tube is made of hydrophilic materials tended to be wetted by water, which can enhance the capillary action. Alternatively, the tube can be made of different types of materials, but coated on its inner surface with a surface coating of materials that tend to be wetted by water.

The sensing element 500 includes a number of metallic contacts. In one embodiment, there are three contacts 504, 506 and 508, with at least two of them positioned internal to the tube 502. The contacts are spaced apart up the tube 502, such as in a linear manner. As an example, the first contact 504 is close to or at the opening of the tube 502. The second contact 506 is at a certain fixed distance from the first contact 504, and the third contact 508 is further up the tube 502. Each contact is connected to a conducting wire or a conductor to electrically extend the contacts out of the tube. For example, as shown in FIG. 9, a first wire 514 connects to the first contact 504, a second wire 516 connects to the second contact 506, and a third wire 518 connects to the third contact 508. In one embodiment, for structural reasons, the wall thickness of the tube 502 increases further away from the opening of the tube. For example, in FIG. 9, the hollow tube 502 inserted inside the mouth is connected through an air-tight joint to another hollow tube 520 that has a thicker wall.

To determine the hydration level of the person, as shown in FIG. 9, a portion of the hollow tube 502 is positioned inside the mouth, probably below the tongue of the user. Then the resistance between at least two of the contacts is measured through their corresponding conductors to determine the hydration level of the user.

There can be different ways to clear the saliva from the tube. One approach is based on a mechanical pump. FIG. 10A shows an embodiment of a re-usable hydration sensor 550 based on a mechanical pump 552. FIG. 10B shows some of the components inside the sensor 550. As in FIG. 9, the sensor 550 includes a channel or a hollow tube 554 with a small inner diameter. Inside the tube 554, there are a number of electrical contacts. In the following example, assume that there are three contacts, similar to the three contacts in FIG. 9, with three wires from the three contacts. The three wires from the three contacts are used to measure the resistances between or among the contacts. In one embodiment, the three wires are connected to three connection points on a printed circuit board 556. In one embodiment, the circuitry on the board 556 includes those shown in FIG. 7A or 7B, with a microcontroller 558. There can also be a LCD display or other types of

16

display for the controller 558. The sensor 550 can be operated by a small battery, such as a coin-cell battery 560.

To clear the saliva inside the tube 554 of the sensor 550 shown in FIG. 10B, the user can press a mechanical pump 552, which can be bellows 562 with a spring 564. When the bellows 562 are pressed down, air is expelled from the sensor 550, pushing any saliva out from the tube 554. In one embodiment, when the bellows 562 are pressed down beyond a certain preset point, a switch 566 is triggered, which activates the circuitry on the printed circuit board 556 to measure the resistance value between at least two contacts.

After being pressed, as the bellows 562 expands, a small vacuum is created. The flow rate of saliva up the tube 554 depends on the sucking force due to the vacuum created, the diameter of the tube and the viscosity of the saliva in the user's mouth. The time elapsed for the saliva to move, such as from the second to the third contact in the tube, is proportional to the vacuum and the saliva viscosity. The viscosity is inversely proportional to mouth hydration. By measuring the time elapsed, the sensor 550 can determine the viscosity of the saliva in the user's mouth.

In one embodiment, the pressure created by the vacuum is constant. This is accomplished through different ways, for example, by using a spring with a constant spring force, or a hollow sphere of rubber (like an eye-dropper bulb) for the bellows. To illustrate, one way to make a spring with a constant spring force is to use a long compression spring of fine spring wire (such as 8" long) and compress the spring into a short spring (such as 0.4" long). The spring force from the compressed spring is substantially constant.

In another embodiment, the pressure created by the vacuum is also measured by a vacuum pressure sensor inside the bellows for determining the viscosity of the saliva.

In one embodiment, there is a hole at the top surface of the bellows. When the bellow 562 is pressed, the finger pressing the bellow 562 covers the hole and air is pushed out of the tube 554. After being pressed, when the bellow 562 expands, the hole is exposed to suck air back into the bellow 562. With the hole being of sufficient size, no vacuum is created. The flow rate of saliva up the tube 554 depends on the viscosity of the saliva in the user's mouth.

In one embodiment, after saliva is removed from the tube by a pump or other methods, there might be a small droplet of saliva still remaining at or hanging onto the opening of the tube. One way to remove the droplet is to wipe the opening of the tube with a piece of cloth to absorb the droplet.

In one embodiment, the sensor shown in FIG. 10B also includes a memory device and a connector. The connector could be a standard USB connector. The memory device can keep track of, for example, the hydration measurements made and the time the measurements were made. Through the connector, one can upload the measurements to another device or instrument to analyze the data. This other device or instrument can be a computer with analysis software.

In one embodiment, a hydration sensing element can be attached to the user, either directly (such as on the user's ear) or onto something worn by the user (such as the user's eye-glasses, hats or clothes). For example, the sensing element can include an attaching mechanism, such as a clip, which can attach the sensing element to the user. In one embodiment, with the element attached or worn, the tube for saliva to move or seep into is allowed to be within the user's mouth. In one embodiment, the sensing element can measure the saliva of the user continually at predetermined intervals.

In one embodiment, the sensing element can also include a wireless transceiver, which is configured to allow information related to the measurements to be wirelessly transmitted to

another electronic device, such as a portable device carried by the user or someone close to the user. In one embodiment, the portable device after analyzing the measurements, wirelessly transmits an indication to the sensing element (e.g. the user needs to drink), and the sensing element can alert the user. Alternatively, the portable device directly provides the indication to the user.

In one embodiment, the portable device can transmit information related to the measurements wirelessly to a remote electronic device (as opposed to, for example, a local device, like a portable device carried by the user). The remote electronic device can be a remote station. For example, if the user is a marathon runner, a remote station can continually monitor and analyze the runner's hydration level. Based on the analysis, if the runner needs to drink, the station can wirelessly send a signal to the portable device, which can then give a signal to the runner. If the portable device is carried by a support team for the runner, the signal will be provided to the support team. The signal can be, for example, a beeping signal, a message or a blinking LED to alert the runner to drink fluid.

In one embodiment, the portable device or the remote electronic device, based on information about the climate and other information, can advise the user or his support team on how much the user should drink at the next water/fluid location. The advise can also depend on the position of water/fluid locations (or other information regarding the race) and the location of the user, which can be identified through a positioning device, such as a global positioning device, carried by the user. In one embodiment, the user's location information can be wirelessly received by the remote station as well.

In one embodiment, the sensing element is connected to a portable device or another electronic device, through a wired connection.

FIGS. 11A-11D show an embodiment of a re-usable hydration sensor 600. It can be similar to the one shown in FIG. 10A. The re-usable hydration sensor 600 can be attached to or worn in the mouth of a user. In this embodiment, the sensor 600 is inside the mouth and is configured to fit on at least one tooth of the user. In one embodiment, the sensor 600, as shown in FIGS. 11A-11D, is a bitable hydration sensor, which can remove saliva from a tube when the user appropriately bites on it.

FIG. 11A shows the bitable sensor 600 inside the mouth of the user. FIGS. 11B-11D show the top, side and rear view of the bitable sensor 600, respectively. The bitable sensor 600 includes a U-shape seat 602, which in the figure is shaped to sit on the lower right first molar. On top of the seat are bellows 604, with a top cover 606. The top surface of the top cover 606 can be shaped to fit the upper right teeth of the user.

As in the embodiment shown in FIG. 10A, saliva gets into a tube 608 of the bitable sensor 600. To remove saliva in the tube, the user can bite on the bellows 604 of the bitable sensor 600. In one embodiment, when the user bites on the bellows 604, the sensor electronics are activated, such as similar to the embodiments shown in FIG. 10B. In another embodiment, the sensor electronics are activated by the tongue pushing an on/off button, which can be on a side surface of the sensor, such as there can be an on/off button on the inner side surface of the U-shape seat 602.

In one embodiment, the bitable sensor 600 further includes a casing 610 that carries circuits for a power source, such as a battery. In another embodiment, the casing also carries a wireless transmitter. After the sensor has taken measurements, the transmitter transmits the measurements to, for example, a portable device, which, for example, can be carried by the user or another. The portable device can analyze

the measurements received and provide feedback to the user, such as he is fine and does not need to drink yet.

In an alternative embodiment, the sensor can be provided in the mouth, but not be bit-activated. In one implementation, the tube or channel for the sensor can be cleared by using one's tongue to depress a bellow. In another embodiment, an electro-mechanical pump can be used to clear the tube or channel of the sensor.

Instead of a mechanical pump, a re-usable hydration sensor can include an electro-mechanical pump to clear saliva from a channel or tube. Under certain condition, the pump is activated electrically to pump saliva from the user's mouth. There are different ways to set the condition. For example, the pump is turned on periodically to clear the tube. In another example, the user can activate a switch to turn on the pump.

FIG. 12 shows an embodiment of different electrical components 630 of a re-usable hydration sensor based on an electro-mechanical pump. Another such pump can also suck saliva into the sensor. The different conditions for activating the one or more pumps in FIG. 12 will be described in the following.

FIG. 12 shows three conducting wires 634, 636 and 638 leading into a microcontroller unit 632. In one embodiment, the three wires can be the three conducting wires from the three contacts of the sensing element shown in FIG. 9. In the following discussion, the three conducting wires are assumed to be three shown in FIG. 9, with 634 corresponding to 514, 636 corresponding to 516, and 638 corresponding to 518. FIG. 13 shows an embodiment of a process 670 for using the electronics of a re-usable hydration sensor such as shown in FIG. 12. First, a pressure pump 644 is turned on 672 to push air through the tube 640, which would clear saliva from the tube 640. With the saliva cleared from the tube 640, the inputs A and B received by the microcontroller unit (MCU) 632 will read high or logic 1. At this instant, saliva is substantially cleared from the tube 640 so the resistances between both the first contact and the second contact, and between the second and the third contacts in the sensing element shown, for example, in FIG. 9 are high. By keeping the pressure pump 644 on for a preset amount of time, the tube 640 remains clear during that period. This amount of time can depend on how often the MCU 632 takes measurements. After waiting 674 that period, the MCU 632 turns off 676 the pressure pump 644 and turns on 678 a vacuum pump 642. The MCU 632 then waits 680 till the reading in its input A becomes low (logic 0). At this instant, the resistance between the first and the second contact, through the first 634 and the second 636 conducting wires, is low (or below a preset value) due to the saliva provided between the contacts. Then the MCU 632 monitors 682 the amount of time "T" till its input B also becomes low (logic 0). At this point, the resistance between the second and the third contacts, through the second 636 and the third 638 conducting wires, is low (or below a preset value), again due to the saliva provided between those contacts. Then the MCU 632 turns off 684 the vacuum pump 642. This time T is proportional to the pressure of the vacuum pump and the viscosity of the saliva. The viscosity inversely depends on how well hydrated the user is. The process 670 is repeatable.

In an embodiment that uses a vacuum pump to pull saliva up a tube or channel, the tube or channel uses hydrophobic materials, which can be more easily cleaned and dried for subsequent use. Examples of materials for the tube or channel include polypropylene or polyethylene.

In one embodiment, the embodiment 630 shown in FIG. 12 does not include a vacuum pump 642. After a preset amount of time of the pressure pump 644 being on, the MCU 632 turns off the pressure pump 644. Saliva, if there is any, moves

up the tube **640** by capillary action. The MCU **632** then waits till the reading in its input A becomes low (logic 0). At this instant, the resistance between the first and the second contact, through the first and the second conducting wires, is low (or below a preset value) due to the saliva provided between the contacts. Then the MCU **632** monitors the amount of time "T" till its input B also becomes low (logic 0). At this point, the resistance between the second and the third contacts, through the second and the third conducting wires, is low (or below a preset value), again due to the saliva provided between those contacts. This time T is proportional to the viscosity of the saliva, which inversely depends on how well hydrated the user is. The process can be repeated.

Instead of using a pressure pump and a vacuum pump, in another embodiment, the user can blow into the tube to clear the pumps.

A number of re-usable sensing elements have been described where there is a small channel, such as in a small tube. In one embodiment, the small channel with electrical contacts is formed using a printed circuit board. There can be a printed circuit board and another board with a trough on one side.

There are different ways to make the board with a trough. For example, a trough can be made as the board is injection molded, by making the trough a feature in the injection mold. Another way to make the trough can be by a milling machine. To illustrate, for example the cross section of the trough is rectangular in shape, whose height and width dimensions are in the order of 5 mils. The board with the trough can be made of thermal plastic or other types of materials, such as silicone or Teflon. The board with the trough can also be, more generally, considered a trough in a substrate. In one example, the substrate can be a type of dielectric material. In another example, there can be a coating over the materials at least in the trough area where the coating tends to be wetted by water.

Regarding the printed circuit board, a number of conducting lines are formed on it. They can function as the conducting wires shown in FIG. 9, such as **514**, **516** and **518**. Then an insulating layer is formed over the lines. This layer can be a plastic layer on the printed circuit board, such as a solder mask. There are holes in the insulating layer for contacts. The conducting lines in the vicinity of the holes can be gold plated, and they can serve as contacts. These contacts can function as the contacts in FIG. 9, such as **504**, **506** and **508**. The gold plating helps prevent corrosion.

The two boards are then joined together, with the trough aligned to the contacts. There are different ways to join the boards together, such as by ultrasonic welding, adhesives or using screws. In another embodiment, the boards are joined together using a double-sided sticky tape, with the tape having a hole in the area of the trough. If the trough is rectangular in cross-section, the walls of the trough can serve as three of the sides, with the printed circuit board serving as the final side of the channel.

In yet another embodiment, a small channel is formed using tapes. For example, after forming the conducting lines on a board, two pieces of tapes are put on the board to serve as the side walls of the channel. Then a piece of acrylic is put on top of the tapes. Different means can be used to hold the structure together. For example, the tapes are double-sided sticky tapes; glue can be applied onto the top of single-sided sticky tapes; or glue can be applied onto the edges of the structure to hold it together. The boundaries of the channel would be the board, the tapes and the acrylic, with the board and the acrylic forming two surfaces and the tapes forming the side walls. The thickness of the tapes determines the

height of the channel. In one example, the thickness of the tapes is 2 mils and the width of the channel is 100 mils. Instead of using tapes as the side walls of the channel, in one embodiment, solder mask or paint is used as the side walls of the channel.

In another embodiment, the piece of acrylic can be molded with two ribs or rails, which serve as the side walls, and which are placed against the circuit board. The structure can be secured with glue on the outside. In this embodiment, one surface and the two sides or walls of the channel are formed by the acrylic piece, and the other surface is formed by the circuit board.

In one embodiment, one or more of the walls or surfaces of the small channel or tube are textured. A matte surface can be more hydrophilic. As an example, at least a portion of the channel is made of acrylic, and the acrylic walls or surfaces are textured. Also, when the matte surface is wet, it is transparent, and when it is dry, it is translucent. Depending on whether an area is transparent or translucent, one can determine whether saliva has moved into the area.

In another embodiment, a small channel can be opened and closed. For example, the channel can be opened by the action of a lever, and closed by the action of a spring. In this example, one can open the channel to wipe it clean and to have it dried.

A number of re-usable hydration sensing elements have been described, each having a channel for saliva to get in. In one embodiment, after such a sensing element has been used, the channels can be cleaned using alcohol, such as rubbing alcohol. For example, the opening of a channel can be immersed in alcohol for a duration of time. By, for example, capillary action, the alcohol goes up the channel. Then the opening of the channel is removed from the alcohol. In one embodiment a pressure pump can be used to remove alcohol from the channel. In another embodiment, the alcohol in the channel is removed by evaporation. The user can perform this operation a few times if desired to further clean the channel.

In yet another embodiment, a hydration sensing element can be based on piezoelectric effect. For example, the element includes a piezoelectric element coupled to a piece of absorbent medium, such as a thin sponge. The medium expands and gets heavier when it absorbs fluid. As the medium expands, the element is flexed, and its electrical impedance changes. The impedance of the piezoelectric element is measured, for example, at an AC frequency by an impedance measuring circuit. The AC frequency can be, for example, approximately 3 kilohertz. The degree of change depends on the expansion of the medium, which depends on the amount of fluid the medium absorbs. The amount absorbed in turn is a function of the viscosity of the saliva in the mouth. Thus, by measuring the impedance or the change in impedance as a function of time, one can determine the dryness of the mouth. To measure the swelling of an absorbent medium using a piezoelectric cantilever over the medium is known in the art, and will not be further described. In one embodiment, such a hydration sensing element is used in a hydration sensor. The sensor can further include different electrical components, such as a controller, a display, a switch and a power source. The controller can monitor the measured impedance or the change in impedance, and convert the monitored results to hydration level, which can be displayed accordingly. The sensor can be handheld, attachable to or mounted on the user, according to different embodiments.

Another type of hydration sensing element that is based on measuring the viscosity of fluid is described in U.S. Pat. No. 6,584,831, which is hereby incorporated herein by reference. This type of element can be incorporated into different types of sensors, as previously described.

21

In one embodiment, a hydration sensor or a hydration sensing element as previously described is calibrated for a user. After the calibration is performed, that type of sensing element or that sensing element can be personalized to the user.

In the following, the sensing element, such as the one shown in FIG. 6A with three conducting lines, is used as an example, though other hydration sensing elements or sensors are applicable. The calibration method can be implemented by a computing device, which can be a handheld device. FIG. 14 shows one embodiment of a calibration process 700.

First, the method 700 suggests 702 the user to be well-hydrated. This can be accomplished, for example, by asking the user to drink 8 ounces of fluid every 2 hours until his urine is clear. When the urine is clear, the user is assumed to be well-hydrated. The suggestion can be through voice, visual or audiovisual techniques from a computing device. Then the method suggests 704 the user to put the sensing element into his mouth, and measures 706 the time T it takes for the user's saliva to wick a preset distance. This can be by measuring the time T when the resistance between the middle conducting line and either or both of the two outer conducting lines drops to a preset value. This time T becomes the reference time or base line of the user. It can be used to indicate the user to be well hydrated. The method then suggests 708 the user to exercise till a user's characteristic changes by a certain percentage. At that point, again the method measures 710 the time T1 for the user's saliva to wick a preset distance, which can be the same preset distance as last time. The method or process can ask the users to continue to exercise until the certain characteristic changes by a second preset value. Again perform the time measurement for the user's saliva to wick the preset distance. This third time T2 will be the time indicating the user is dehydrated to a point where the user's characteristic has changed by the second preset value. This process can repeat by continuing to ask the user to exercise. After the measurements, the sensor is calibrated for the user. Note that instead of measuring the time for a preset distance of wicking, in another approach, the method can measure the distance wicked for a preset amount of time.

In the calibration process, the user's characteristic or attribute can be the user's weight. As an example, the user can ride a stationary exercise bicycle for a duration of time, such as 15 minutes. Then, the user gets off the bike, removes sweat with a towel and measures his weight with an accurate scale. The user keeps doing this until his weight drops by such as a certain percentage. The time T1 can indicate that the user is dehydrated to the point where the user has lost 0.5% of weight, and the time T2 is where the user's weight loss is 1%. In the future, by measuring the time for saliva to wick the preset distance, the sensing element would be able to indicate how much fluid relative to the person's weight the user needs to drink just to replenish his weight loss due to, for example, dehydration.

Instead of using weight loss, in another embodiment, another attribute of a user can be measured to calibrate a hydration sensor. For example, instead of measuring weight loss, the body temperature of the user is measured to calibrate a hydration sensor.

The calibration process can be performed with respect to a type of sensing element for a group of users. The group of users might have certain similar characteristics because the calibration results might depend on the certain similar characteristics of the users, such as weight and age. For example, all of them are normal-weight adults, or all of them can be 30% over weight. Using the same approach as above, for example, in FIG. 14, the method averages the time measured

22

for all of the users at each step. For example, the average time T1 would be the time indicating a user in that group using that type of sensing element being dehydrated by 0.5% of the users' weight. Then, in the future, by measuring the time for saliva to wick the preset distance for that type of sensing element and for users with the similar characteristics, the sensing element would be able to indicate how much fluid relative to a user's weight that the user needs to drink just to replenish his weight loss due to, for example, dehydration.

In one calibration process, a timer measures the time elapsed for a fixed distance wicked by saliva. This process is applicable for many of the different types of sensing elements and sensors previously described, such as the ones shown in FIGS. 1C, 2, 3A, 4, 5B. In yet another embodiment, instead of measuring time elapsed for a fixed distance wicked by saliva, a hydration sensing element can measure the distance wicked by saliva during a fixed time. This approach is applicable, for example, for the sensing elements or sensors shown in FIGS. 1C, 2, 4 and 5B.

In one embodiment, a hydration sensor includes a hydration sensing element to determine the optimal amount of fluid a user should consume in order for the user to be well-hydrated. The sensing element can have been calibrated by a method as described above. Then, based on measuring the hydration level of the user with the element, the sensor determines the optimal level of fluid the user should consume for the user to be well hydrated, and provide a recommendation to the user.

In another embodiment, the optimal amount of fluid to be consumed for a user can also depend on other factors of the environment a user is in. For example, a hydration sensor includes a hydration sensing element (such as one of the elements disclosed) and an environmental sensor that senses an attribute of the environment the user is in. FIG. 15 shows examples of environmental sensors applicable for appropriate hydration measurements according to different embodiments. For example, a temperature sensor can be configured to measure the temperature of the environment where the user is in, and the sensor is coupled to a hydration sensing element. As another example, a humidity sensor (coupled to a hydration sensing element) is configured to sense the humidity of the environment of the hydration sensing element. Based on one or more of these additional environmental sensors, the hydration sensor determines the optimal amount of fluid the user should consume. In one embodiment, after the determination, the sensor provides a recommendation to the user. The recommendation can be, for example, visual or audio.

In yet another embodiment, the optimal amount of fluid to be consumed can depend on one or more additional attributes regarding the user, other than the hydration level of the user. In one embodiment, a hydration sensor includes a hydration sensing element (such as one of the sensing element as disclosed) and a user-attribute sensor that measures an attribute of the user other than the user's hydration level. The optimal amount of fluid the user should consume depends on both the measurements by the hydration sensing element and by the user-attribute sensor. For example, one user-attribute sensor is a temperature sensor for sensing the temperature of the user. Another is a position sensor for identifying the location of the user. Yet another example for a user-attribute sensor is an activity sensor, such as a pedometer, for sensing the activity level (or the lack of activity) of the user.

Information from such one or more additional sensors can be used to adjust the signal for the user or to help determine the appropriate amount of fluid the user should consume. For example, if the temperature is around 72 degrees Fahrenheit, the time as measured by a hydration sensor indicating that the

person needs to replenish 0.5% of his body weight of fluid is T1. If the temperature of the environment is high, such as more than 100 degrees, the hydration sensor automatically shortens the time based on a predetermined value.

As shown in a number of embodiments, such as the one shown in FIG. 1B, at least one surface of the sensing element can be made of a piece of opaque materials. In one embodiment, promotional materials or different designs can be printed on that surface. In another embodiment, there can be promotional materials on the sensor. In yet another embodiment, promotional materials can be on a bottle coupled to a hydration sensing element, such as the one shown in FIG. 2.

In one embodiment, the hydration sensing element or sensor is incorporated into a structure that is in the shape of, such as, a spoon, a small cup, or a small container. To use such a sensor or sensing element to measure a user's degree of hydration, as an example, the user spits his saliva into the sensor, such as in the shape of a spoon, to measure the saliva.

In one embodiment, the hydration sensing element, such as the one shown in FIGS. 1A-1D, can be incorporated into a holder of a specific configuration, such as a handle or a stick. For example, a user can hold onto the holder with the sensing element attached to one end of the holder.

In one embodiment, there is a RFID tag coupled to or integral with a hydration sensor or sensing element. The tag can be used to provide, for example, an identification of the sensor, or the tag can be used to transmit wirelessly measurements from the sensor to another device.

In one embodiment, a hydration sensor also provides recommendation to a user using it to be aware of other factors that can affect hydration measurements. For example, an audio signal can tell the person to avoid eating food such as candies or chewing gums, or drinking any beverages, right before taking measurements because such food or water might affect saliva flow, which in turn would distort the hydration measurements.

A number of embodiments have been described where saliva flows into a channel, which can be a minute channel, through capillary effect. Other embodiments have also been described where saliva flows into a channel with the assistance of a vacuum pump, which can be a mechanical or electro-mechanical pump. In one embodiment, with the pump, the dimension of the channel can be larger because saliva flows up the channel not just based on capillary effect.

One or more types of hydration sensing elements or sensors can be used to provide an absolute index on the hydration level of a user. One approach to determine absolute index based on a sensing element is to compare the known viscosity of certain liquids (known standards) with the measured results. A standard curve can be obtained from the viscosities of the known standards. The measured results are then fitted to the standard curve to determine an equation or to create a table that correlates the measured results to the standard curve. In the future, based on the equation or the table, the absolute viscosity value can be determined from the sensor measurements.

Certain disease can also affect the accuracies of the measurements. For example, a person with dry mouth or xerostomia may not give accurate result. Xerostomia could be due to genetic, radiation therapy, blood-pressure medication and autoimmune diseases. In one embodiment, a hydration sensor would warn or alert the user that if the user has sicknesses such as dry mouth, the measurements may not be an accurate measurement of his hydration level.

In yet another embodiment, a hydration sensor or sensing element, such as one or more of the previously described ones, is used for measuring symptoms related to the disease

xerostomia or dry mouth of a user. Typically, the normal flow rate of saliva in an unstimulated manner is about 0.3 to 0.5 mL/minute. Values less than 0.1 mL/min are typically considered xerostomic. Flow rate and viscosity are related. In one embodiment, by measuring viscosity using, such as a viscosity sensor or sensing element as described, one can tell if a person has xerostomia. In another embodiment, the sensor or sensing element has previously been calibrated by a method as described, and the calibration can be for the person being measured.

In one embodiment, a hydration sensor or a hydration sensing element electrically couples to a bottle. In another embodiment, different electrical components in the sensor or sensing element can be incorporated in the bottle. Different embodiments regarding electrical components in a bottle have previously been described in one or more of the related patent applications identified above and incorporated by reference.

The various embodiments, implementations and features of the invention noted above can be combined in various ways or used separately. Those skilled in the art will understand from the description that the invention can be equally applied to or used in other various different settings with respect to various combinations, embodiments, implementations or features provided in the description herein.

A number of embodiments in the invention can be implemented in software, hardware or a combination of hardware and software. A number of embodiments of the invention can, at least in part, be embodied as computer readable code on a computer readable medium. The computer readable medium is any data storage device that can store data which can thereafter be read by a computer system. Examples of the computer readable medium include read-only memory, random-access memory, CD-ROMs, magnetic tape, optical data storage devices, and carrier waves. The computer readable medium can also be distributed over network-coupled computer systems so that the computer readable code is stored and executed in a distributed fashion.

Numerous specific details are set forth in order to provide a thorough understanding of the present invention. However, it will become obvious to those skilled in the art that the invention may be practiced without these specific details. The description and representation herein are the common meanings used by those experienced or skilled in the art to most effectively convey the substance of their work to others skilled in the art. In other instances, well-known methods, procedures, components, and circuitry have not been described in detail to avoid unnecessarily obscuring aspects of the present invention.

Also, in this specification, reference to "one embodiment" or "an embodiment" means that a particular feature, structure, or characteristic described in connection with the embodiment can be included in at least one embodiment of the invention. The appearances of the phrase "in one embodiment" in various places in the specification are not necessarily all referring to the same embodiment, nor are separate or alternative embodiments mutually exclusive of other embodiments. Further, the order of blocks in process flowcharts or diagrams representing one or more embodiments of the invention do not inherently indicate any particular order nor imply any limitations in the invention.

Other embodiments of the invention will be apparent to those skilled in the art from a consideration of this specification or practice of the invention disclosed herein. It is intended that the specification and examples be considered as exemplary only, with the true scope and spirit of the invention being indicated by the following claims.

25

The invention claimed is:

1. A hydration sensor for measuring the hydration level of a user based on the user's saliva, comprising:

a digital timing device providing a timing indication; and
a disposable sensing element including:

a piece of water-permeable material having a first side
and a second side, with a chemical compound coupled
to the first side;

a first piece of water-impermeable material coupled to
the first side of the water-permeable material, over the
chemical compound; and

a second piece of water-impermeable material coupled
to the second side of the piece of water-permeable
material,

wherein the disposable sensing element does not include
an electronic device,

wherein the disposable sensing element includes at least
one aperture that allows saliva in the mouth of the user
to reach the water-permeable material, and to the
chemical compound via the water-permeable material,

wherein the chemical compound is configured to change
color of at least a portion of the water-permeable
material due to contact with saliva and the change is
observable from at least a portion of one piece of the
water-impermeable material,

wherein at least a portion of the disposable sensing element
is configured to be placed in the mouth of the
user to measure the hydration level of the user, and the
disposable sensing element may be disposed after the
element has been placed in the mouth of a user to
measure hydration level, and

wherein the hydration sensor further includes an indicator,
the indicator to provide an indication for the hydration
level of the user, based on time measurement regarding
color change of the at least a portion of the water-permeable
material, after the disposable sensing element is
placed in the mouth of the user, via the timing indication.

2. A hydration sensor as recited in claim 1, wherein the
chemical compound extends along a certain distance on the
water-permeable material, and the indication depends on the
extent of the color change of the water-permeable material
along the certain distance after the disposable sensing element
is placed in the mouth of the user.

3. A hydration sensor as recited in claim 1, wherein the
at least one aperture includes at least an edge of the water-
permeable material that is exposed so that saliva is allowed to
reach the chemical compound through the edge of the water-
permeable material, or an opening on the first or the second
piece of water-impermeable material so that saliva is allowed
to reach the chemical compound through the opening.

4. A hydration sensor as recited in claim 1,
wherein at least two types of chemical compounds are
coupled to the first side of the water-permeable material,
and

wherein the color change of the water-permeable material
due to the at least two types of chemical compounds is
different as saliva contacts with them.

5. A hydration sensor as recited in claim 1, wherein the
chemical compound is selected from the list consisting of a
powder food dye, a non-toxic water-based paint, and a non-
toxic and hypoallergenic compound.

6. A hydration sensor as recited in claim 1, wherein the
indicator includes at least a LED and a photodiode to measure
color change of the water-permeable material.

7. A hydration sensor as recited in claim 1, wherein at least
the digital timing device of the sensor is in a carrier, which

26

includes a mechanical device configured to attach the carrier
to a piece of clothing worn by the user.

8. A hydration sensor as recited in claim 1,
wherein the disposable sensing element is connected to a
plurality of similar elements to form a stack, and
wherein each of the elements of the stack is configured to
be used individually for measuring hydration level.

9. A hydration sensor as recited in claim 1,
wherein the sensor is configured to be handheld, and
wherein the indicator comprises electrical components to
sense the change in color of the water-permeable material.

10. A hydration sensor as recited in claim 1 further com-
prising another sensor configured to measure either another
attribute of the user or an attribute of the environment where
the user is in, wherein the indication regarding the hydration
level of the user is also based on measurements from the
another sensor.

11. A disposable hydration sensing element for measuring
the hydration level of a user based on the user's saliva, com-
prising:

a piece of water-permeable material having a first side and
a second side, with a chemical compound coupled to the
first side;

a first piece of water-impermeable material coupled to the
first side of the water-permeable material, over the
chemical compound; and

a second piece of water-impermeable material coupled to
the second side of the piece of water-permeable material,

wherein the disposable hydration sensing element does not
include an electronic device,

wherein the disposable hydration sensing element includes
at least one aperture that allows saliva in the mouth of the
user to reach the water-permeable material, and to the
chemical compound via the water-permeable material,
wherein the chemical compound is configured to change
color of at least a portion of the water-permeable material
due to contact with saliva and the change is observable
from at least a portion of one piece of the water-impermeable
material,

wherein at least a portion of the disposable sensing element
is configured to be placed in the mouth of the user to
measure the hydration level of the user,
wherein the disposable hydration sensing element further
includes an indicator, the indicator to provide an indication
for the hydration level of the user, based on an
amount of time regarding color change of the at least a
portion of the water-permeable material, after the disposable
hydration sensing element is placed in the mouth of the user, and

wherein the hydration sensing element may be disposed
after the element has been placed in the mouth of a user
to measure hydration level.

12. A disposable hydration sensing element as recited in
claim 11, wherein the chemical compound extends along a
certain distance on the water-permeable material, and the
indication depends on the extent of the color change of the
water-permeable material along the certain distance after the
disposable hydration sensing element is placed in the mouth
of the user.

13. A disposable hydration sensing element as recited in
claim 11, wherein the at least one aperture either includes an
edge of the water-permeable material that is exposed so that
saliva is allowed to reach the chemical compound through the
edge of the water-permeable material, or includes an opening

on the first or the second piece of water-impermeable material so that saliva is allowed to reach the chemical compound through the opening.

14. A disposable hydration sensing element as recited in claim 11,

wherein at least two types of chemical compounds are coupled to the first side of the water-permeable material, and

wherein the color change of the water-permeable material due to the at least two types of chemical compounds is different as saliva contacts with them.

15. A disposable hydration sensing element as recited in claim 11, wherein the chemical compound is selected from the list consisting of a powder food dye, a non-toxic water-based paint, and a non-toxic and hypoallergenic compound.

16. A disposable hydration sensing element as recited in claim 11,

wherein the disposable hydration sensing element is connected to a plurality of similar elements to form a stack, and

wherein each of the elements of the stack is configured to be used individually for measuring hydration level.

* * * * *